

524 779

10/524779

(12) INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(19) World Intellectual Property  
Organization  
International Bureau



(43) International Publication Date  
26 February 2004 (26.02.2004)

PCT

(10) International Publication Number  
**WO 2004/017061 A1**

(51) International Patent Classification<sup>7</sup>: **G01N 27/447**,  
21/05

(21) International Application Number:  
PCT/GB2003/003591

(22) International Filing Date: 15 August 2003 (15.08.2003)

(25) Filing Language: English

(26) Publication Language: English

(30) Priority Data:  
0219248.2 17 August 2002 (17.08.2002) GB

(71) Applicant (for all designated States except US): **UNIVERSITY OF YORK** [GB/GB]; Research & Industry Office, The Innovation Centre, York Science Park, Heslington, York YO10 5DG (GB).

(72) Inventors; and

(75) Inventors/Applicants (for US only): **GOODALL, David, Murray** [GB/GB]; Department of Chemistry, University of York, Heslington, York, YO10 5DD (GB). **BERGSTROM, Edmund, Thomas** [GB/GB]; Department of Chemistry, University of York, York, YO10 5DD (GB). **ALLINSON, Nigel, Martin** [GB/GB]; Stonebridge

House, Selby Road, York, YO19 4RD (GB). **MOON, Kevin, James** [GB/GB]; 1 Heather Bank, Osbaldwick, York, YO10 3QH (GB).

(74) Agent: **NOVAGRAAF PATENTS LIMITED**; The Crescent, 54 Blossom Street, York YO24 1AP (GB).

(81) Designated States (*national*): AE, AG, AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, BZ, CA, CH, CN, CO, CR, CU, CZ, DE, DK, DM, DZ, EC, EE, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, MZ, NI, NO, NZ, OM, PG, PH, PL, PT, RO, RU, SC, SD, SE, SG, SK, SL, SY, TJ, TM, TN, TR, TT, TZ, UA, UG, US, UZ, VC, VN, YU, ZA, ZM, ZW.

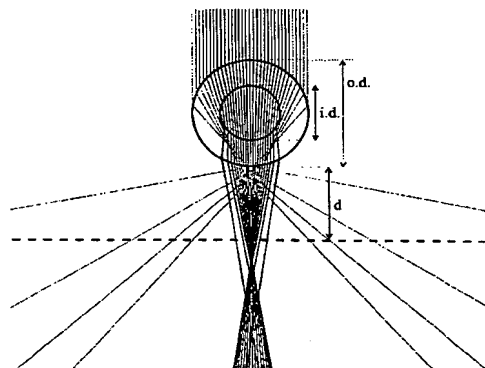
(84) Designated States (*regional*): ARIPO patent (GH, GM, KE, LS, MW, MZ, SD, SL, SZ, TZ, UG, ZM, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, BG, CH, CY, CZ, DE, DK, EE, ES, FI, FR, GB, GR, HU, IE, IT, LU, MC, NL, PT, RO, SE, SI, SK, TR), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW, ML, MR, NE, SN, TD, TG).

Published:

- with international search report
- with amended claims

[Continued on next page]

(54) Title: OPTICAL ASSEMBLY AND METHOD FOR DETECTION OF LIGHT TRANSMISSION



Water-filled capillary 100 µm i.d., 194 µm o.d.

(57) Abstract: An optical assembly comprising a light source, at least one sample vessel and a detector, the at least one vessel being positioned in a light path or paths created between the source and the detector in manner to enable transmission of light through the vessel wherein the light source is adapted to provide a beam of substantially collimated light, the detector comprises a plurality of detector locations and the vessel comprises a wall and core of relative shape and dimensions adapted to contain a sample for detection and to define at least two spatially separated transmitted light paths, a first wall path which enters and exits the vessel walls only, spatially separated from a second core path which enters and exits the vessel walls and additionally the vessel core, wherein the spatially separated wall and core paths are coupled to individual detector locations on the detector, a module or clip-on device therefor, method for detection and uses thereof.

BEST AVAILABLE COPY

WO 2004/017061 A1



*For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.*

## OPTICAL ASSEMBLY AND METHOD FOR DETECTION OF LIGHT TRANSMISSION

The present invention relates to an optical assembly comprising a sample  
5 vessel positioned in a direct light path between a light source and a light  
detector, in manner to enable transmission of light through the vessel; a  
method for detection of light transmission through sample contained within  
the vessel; an apparatus comprising the assembly; more particularly an  
apparatus for sample analysis for example for high throughput screening  
10 (HTS) or profiling or assays, such as enzyme assays; and uses thereof in the  
pharmaceutical, biomedical and bioscience, agrochemical, veterinary,  
materials and like fields, for detection, analysis, characterisation and  
quantification or the like of samples contained in a vessel, and optionally  
further collecting separated components thereof; in particular in combinatorial  
15 chemistry; in metabolomics, proteomics or genomics, assay and high  
throughput analysis applications, typically high sensitivity analyses, separation  
and/or quantification studies and for sample separation for example  
chromatography or electrophoresis, in particular column chromatography,  
capillary electrophoresis with real time or post separation analysis.

20 UV absorbance, fluorescence and mass spectrometry are key technologies  
used in separation science for analysing species in samples. A particularly  
useful methodology is to look at a sample population separated by capillary  
electrophoresis with fluorophore labelling and fluorescence imaging, for  
25 quantification, and MS for characterising molecules of interest.

US 5,582,705 discloses an apparatus and system for laser induced  
fluorescence (LIF) detection in a multiplexed capillary electrophoresis system.  
A coherent beam incident on the capillary array and emitted fluorescent light

are typically perpendicular to each other in order to reduce background noise due to light scattering. A transparent portion in each capillary wall defines a transparent path extending through the array, perpendicular to the capillary. A 2D image array detector such as a charge-coupled device (CCD), preferably a charge-injection device (CID), is positioned to detect emission, and an imaging lens interposed between the capillary array and the image array detector, to optically couple the pixels to the capillary. The imaging lens may be any lens capable of transforming an image onto the pixels of the image array detector, such as a camera lens or a condenser lens. Coupling is shown in Figure 4, of US 5,582,705 in which every second pixel is coupled to a sidewall of the capillary and every pixel in between is coupled to an interior portion.

Fluorescence detection is limited in its application since only a limited number of molecules are naturally fluorescent and many have to be derivatised in reproducible and quantitative manner. Absorbance detection therefore has the advantage of enabling detection of a wider range of molecules. For example in enzyme assays, conducted in microtitre wells, techniques can be extended to absorbance detection of chromophoric, UV and vis absorbing substrates consumed or produced in an assay, extending the range of assay to natural as well as synthetic substrates.

However a limitation of absorbance detection lies in the operable wavelength of detection. Absorbance detection is conducted on substrates in solution. However many common solvents absorb significant amounts of light at wavelengths below ~200 nm, and the resulting solvent absorption signal distorts and masks signals resulting from the substrate to be detected. Accordingly absorbance detection is in practice limited to detection at wavelengths in excess of 190 nm, in the range UV-vis to near infra-red (NIR).

Moreover a fundamental limitation of single point absorbance detection is the impossibility of creating an image of the source at the detection point on capillary that is brighter than the light source. In "A charge coupled device array detector for single-wavelength and multi-wavelength ultraviolet absorbance in capillary electrophoresis", Bergström and Goodall, Pokric and Allinson, Anal. Chem. 1999, 71, 4376-4384 discloses optical detection in capillary electrophoresis by means of absorbance detection, illuminating a length of the capillary using a fibre optic bundle and using a charge coupled device (CCD) camera to image the full length of the illuminated zone. In this publication light from a fibre optic bundle is focused by a sapphire rod through the capillary core and detected on the opposite side of the capillary, by this means, increasing the target light area enabling more of the lamp output to be used and increasing the total light flux. In this case light emanates from the capillary core, so all light detected is useful and the divergent beam obtained is imaged on to the CCD.

Such a system becomes more complex once a parallel capillary array is introduced in place of the single capillary. Optics to focus light on the core of each capillary would be extremely complex and therefore irradiating both the core and walls of each capillary becomes a practical consequence.

WO 01/18528 (Yeung et al) discloses a method for analysing multiple samples simultaneously by absorption detection of samples in a planar array of multiple containers, whereby stray light from adjacent containers is eliminated by distancing the detection means from the array, preferably at a distance greater than 10 times the diameter of a container, suitable 10-100 times the diameter for example at a distance of 1-30 cm. Containers are preferably cylindrical capillary tubes as shown in the art. The array comprises a control container if the light source is unstable. It is stated that the cross section of the

container and thickness of the capillary wall are not critical. A flat field lens preferably images the containers on to the detection means.

We have now found that further improvements in absorbance detection  
5 assemblies enables increasing the total light flux through a capillary or other sample vessel, by virtue of simplification of optical components, without unduly large separation of capillary and detector which is undesirable and reduces light collection efficiency compromising path length, and therefore light intensity. The improved assembly is of particular advantage in detection  
10 in multiplexed capillary arrays and enables imaging a large area of a capillary array without the need for imaging optics. This is a significant advantage, especially when working in UV for which it is very difficult and expensive to produce suitable optics. The assembly has benefits however in both single capillary and array detection, in particular enabling a simple and improved  
15 exposure referencing and acceptably low intercapillary cross talk without the need for optics. In addition a benefit of the assembly of the invention is that it is suitable for operation at short pathlengths, by virtue of the increased total light flux through the core of the capillary or other sample vessel, and this reduction in pathlength may lead to opportunities to conduct absorbance  
20 detection at lower wavelengths, less than 190 nm, without encountering impracticably high levels of solvent absorption.

Accordingly there is provided in the broadest aspect of the invention an optical assembly comprising a light source, at least one sample vessel and a detector,  
25 the at least one vessel being positioned in a light path or paths created between the source and the detector in manner to enable transmission of light through the vessel wherein the light source is adapted to provide a beam of substantially collimated light, the detector comprises a plurality of detector locations and the vessel comprises a wall and core of relative shape and

dimensions adapted to contain a sample for detection and to define at least two spatially separated transmitted light paths, a first wall path which enters and exits the vessel walls only, spatially separated from a second core path which enters and exits the vessel walls and additionally the vessel core, wherein the spatially separated wall and core paths are coupled to individual detector locations on the detector.

Preferably the detector is an array detector. Preferably the detector is adapted to detect and provide information on respective wall and core path light transmission. Preferably the assembly is coupled to means for displaying information on respective wall and core path light transmission or for displaying referenced information on core path light transmission, referenced against wall path light transmission.

Preferably the assembly defines a central core path and two peripheral wall paths either side thereof or an annular wall path thereabout. Paths may overlap on emerging from the vessel and at greater separations from the vessel. Preferably the wall and core paths are coupled to detector locations at a vessel outer wall to detector separation or distance  $d$  at which the paths are spatially separated, preferably giving more than 90% separation of core and wall beam fluxes. The assembly may position the vessel in two or more separate light paths to generate two or more sets of spatially separated transmitted light paths coupled to two or more detectors or detector zones.

Preferably the assembly is characterised by internal vessel dimension or path length in the range of 3  $\mu\text{m}$  to 20 mm, external vessel dimension in the range 4  $\mu\text{m}$  to 30 mm, refractive index of vessel wall in the range 1.3 - < 1.6, vessel outer wall to detector separation  $d$  in the range 10  $\mu\text{m}$  to > 300 mm and is for use in detecting a sample comprising analyte in solvent having refractive

- index in the range 1.3 to in excess of 1.5. Reference herein to a sample is to vessel contents which may comprise a single or multiple components. Multiple components may be present as a homogeneous or heterogeneous mixture, and may undergo migration with time ie may be a plurality of liquid phase components optionally including a dissolved phase component; or may include one or a plurality of analytes which it is desired to detect in one or a plurality of solvents or like bulk phase sample component, for example in the course of a chemical reaction generating or consuming a species as analyte.
- 10 In a particular advantage, the apparatus of the invention enables exposure referencing of a light beam traversing a core path of the at least one sample vessel, by a light beam traversing a wall path of the same sample vessel. The beams are spatially close, preferably adjacent, on the array detector, facilitating direct referencing as the ratio of the core beam to the wall beam. In
- 15 a further advantage the two light beams are of neighbouring origin whereby core and wall beams have a high probability of emanating from the same region in the light source eliminating the effects of light source fluctuations due to e.g. instability or spatial inhomogeneity. The assembly of the invention is therefore able to operate at the shot noise limit.
- 20 Preferably the light source comprises any active or passive light source, for example light may be generated at the source or it may be transmitted to the source and emanate therefrom, for example it may be transmitted by an optical fibre to the light source. Preferably the light source comprises at least one
- 25 wavelength of light that is absorbed by one or more absorbing species, the absorbance of which is to be detected. For example the light source output may be coupled from a fibre optic if desired for illumination from a remote light generator or may be coupled from a point to line optical fibre for zone illumination. Coupling the output into a single optical fibre reduces noise



contributions caused by fluctuations in the spatial distribution of the lamp discharge.

Light may be of wavelength in the range 160 to 1200 nm, preferably 180 or  
5 190 to 1200 nm, corresponding to UV, UV-vis to near infra red (NIR), and is preferably in the range 180 to 700 nm corresponding to UV-vis. It is a particular advantage that the present invention enables high sensitivity absorption detection at lower path length in the range 3 - 500  $\mu$ m and this  
10 allows operation at lower wavelengths in the range 160 to 190 nm corresponding to UV which would be impractical for absorbance detection of samples in some solvents by known techniques. Accordingly the method is more solvent independent than normal HPLC or spectrophotometric methods.

A light source may be a point or line source adapted to illuminate a section  
15 through a compact vessel or elongate vessel. A light source may be of single wavelength or multiple discrete wavelengths or wavelength range. A light source may be a tuneable light source, giving a tuneable smooth output, a line output lamp giving a very intense output at one wavelength only, a spectrum light source giving a wavelength range along the length of a line light source  
20 or the like; and may be continuous in time, or pulsed. Sources with continuous outputs are preferable when spectra are to be acquired over a wavelength range. Line sources typically provide more intense outputs at characteristic wavelengths, and are beneficial when the samples absorb at these wavelengths. Wavelength selection in the case of continuous wavelength arc  
25 lamps for example, is suitably by known technique such as interference filter positioned between the light source and collimating means or between the collimating means and the sample vessel, preferably before the collimating means. Alternatively a filter wheel or variable interference filter may be employed for sequential wavelength detection at multiple discrete

wavelengths, or a wavelength dispersing device may be employed in the form of a monochromator such as a grating or prism which may be either fixed in position or continuously variable and spreads light into a spectrum, giving a varied wavelength along the length of the capillary or at right angles to the length of the capillary.

Preferably a light source comprises an iodine, zinc, cadmium or mercury lamp, or laser, as line sources; or a deuterium, xenon or tungsten lamp as continuous output lamp; or a xenon lamp as a pulsed output lamp.

More preferably the light source comprises a deuterium arc lamp (for UV light absorption) or a xenon arc lamp (for UV-vis light absorption); or comprises a tungsten lamp, more preferably a filament lamp (for visible light absorption), and the like; most preferably a high output arc lamp selected from deuterium, iodine, zinc, cadmium, mercury or xenon above; or the light source comprises a line source, preferably for the UV one of the following: iodine, zinc at 214 nm, cadmium at 229 nm, or mercury at 185, 254 or 365 nm; or the light source comprises a laser, for example in the UV a laser such as a frequency quadrupled Nd:YAG at 266 nm or Nd:YLF at 262 nm, or a He-Cd laser at 325 nm.

The light source may be expanded and recollimated by known means, for example using cylindrical and spherical lens elements and the like, preferably using an elongate lens or cylindrical optical component, such as a cylindrical fused silica lens or the like, to produce a collimated beam suitable for zone illumination of a sample vessel array.

The at least one sample vessel in the assembly of the invention may comprise a cell or conduit which may be closed or open ended and closed-or-open based and topped, intended for static or dynamic sample detection. The vessel may

be aligned for light transmission in any suitable plane through the vessel. Suitably light transmission is through a plane perpendicular to or containing the vessel ends or base and top.

- 5 Preferably the sample vessel is a single cell or one of a plurality of cells in an array, such as a rectangular or square array, for example in a microtitre plate, well plate or multi sample plate; or is a capillary, such as a microcapillary or microfabricated channel as known in the art of microfluidic transport and separation, more preferably is a single capillary or microchannel or one of a
- 10 plurality of capillaries or microchannels in a parallel array.

A sample vessel array is aligned in a plane perpendicular to the collimated light path whereby light passes through one vessel only. In the case that direction of illumination is in a plane containing the vessel base and top, light

15 enters and exits each vessel through a sidewall (wall path) or enters through the top and exits through the base (core path), and in this case vessels may be aligned in a parallel or matrix array; in the case that illumination is through a plane perpendicular to the vessel ends, light enters and exits each vessel through a near side sidewall (wall path) or enters and exits through a nearside

20 sidewall, emerges into the core, enters and exits an opposing sidewall (core path), and in this case vessels may be aligned in a parallel array, ie only one vessel deep.

For 1:1 illumination:detection, the collimated light path has dimensions

25 substantially corresponding to the dimensions of width and length of the detector array and to a desired width and length of each sample vessel which it is desired to optically detect. Illumination:detection magnification is preferably in the range 0.8 – 1.5:1 in the case of arrays to avoid problems with spatial overlap of light from neighbouring vessels, and is in the range 0.5 – 2:1

30 for single vessels.

Light passing through the vessel walls and core is refracted on entering and exiting the wall(s) and additionally on entering and/or exiting the core. In the case of illumination through the length of a cell or capillary, or through the cross-section of a straight walled cell or capillary, emergent wall and core light paths maintain their respective orders, ie there is substantially no cross-over or convergence of respective paths, at least at a distance  $d$  from the vessel outer wall to the detector.

10 In a particular embodiment of the invention the vessel of the assembly is a microfabricated device providing square cross section capillaries, and is suitable for Fabry-Perot illumination with enhanced light absorption through multiple passages through the vessel. In this case the walls of the vessel are coated with a reflective coating, within an absorption zone, whereby light enters the vessel core in an illumination zone adjacent the absorption zone, through a nearside side wall, at an angle less than 90 degrees to the wall, and at least a portion of light is reflected at the opposing wall, with repeated internal reflections throughout the absorption zone and finally emergence from the opposing wall at the end of the absorption zone. Light traversing a wall path may be similarly reflected for ease of alignment but is preferably not reflected and exposure referencing is performed as normal.

In the case of illumination through the cross-section of a curved walled cell or capillary, for example a circular cross-section capillary, emergent wall light paths reverse their respective orders about a central core light path, ie there is cross-over of respective wall paths, within a distance  $d$  to the detector. In this case the optical assembly of the invention is characterised by refraction patterns through the vessel in order to be able to spatially separate wall and core light paths. Preferably the assembly is characterised by respective outer and inner diameter of a sample vessel, and by respective refractive indices of

vessel walls and of sample, whereby the wall and core paths are spatially separated as hereinbefore defined.

5 Preferably the refractive index of the vessel wall is greater than that of the bulk phase of any sample comprised in the core. Preferably refractive index of the wall is in the range 1.34 – 1.59. Preferably refractive index of bulk phase sample comprised in the core is in the range 1.32 - 1.48 more preferably 1.32 – 1.38. The refractive index of vessel wall may be modified by cladding or otherwise incorporating higher refractive index material in the vessel wall as a  
10 wall section, lens or the like.

Preferably the vessel outer wall and inner wall are additionally of shape and dimension whereby light transmitted through the core is convergent and forms a beam having an undeflected beam path, i.e. having a beam path continuous  
15 with the incident collimated light. Light passing through the wall of the sample vessel only, entering the wall at one outside wall location and exiting at a second outside wall location may be deflected or undeflected, preferably if deflected is divergent with respect to the core light path such that two classes of light paths are formed which are spatially separated.

20 It will be appreciated that by virtue of using a collimated light source and knowing the refractive index of the sample vessel and any sample contained therein the light path passing through any point of the vessel can be predicted for any given shape and dimension of vessel outer wall and inner wall, chosen  
25 such that collimated light passing through a square or rectangular cross section vessel, normal and parallel to respective walls, emerges substantially unrefracted and parallel; and collimated light passing through a curved or angular cross section vessel emerges uniformly divergent or convergent with a gradation in angle of refraction. This enables production of an emergent light

path of high symmetry and/or uniformity, which can be manipulated for imaging and exposure referencing as hereinbefore defined.

Preferably the at least one sample vessel has a cross-section in a plane including the transmission light path, which is square or rectangular, curved circular or angular or a combination thereof and is symmetrical or asymmetrical, preferably is symmetrical. The sample vessel moreover comprises an outer and inner wall which may be of similar cross-section or shape or may be different, for example one may be circular and one square.

The sample vessel wall through the cross-section may be continuous or non-continuous, for example the vessel may be open or closed and is preferably closed. A closed vessel may have a continuous wall through its cross-section or may comprise continuous base and side walls with a separate seal or lid. Preferably the outer wall is square open or closed or circular closed, and the inner wall is square or well shaped open or closed or is essentially square with microfabricated convex or concave inner wall sections acting as lens faces, or concave, convex or prism shaped outer wall sections acting as lens faces.

Preferably at least one of the outer and inner walls of the sample vessel is of circular cross-section, whereby refraction and spatial separation of core and wall beams is achieved, preferably outer and inner walls are of coaxial circular cross-section thereby defining an annular wall having outer and inner diameters such that refraction and spatial separation of core and wall beams is achieved.

It will be appreciated that sample vessel dimensions, refractive indices and/or vessel to detector distance may be selected according to the nature of vessel wall material and shape and the sample to be contained within the core in order to achieve the desired refraction and spatial separation. Accordingly the

apparatus is defined by a relation of the following properties which are shown here as a flow scheme rather than as a mathematical relation:

$$\frac{i.d.}{o.d.} + r.i.(solvent) + r.i.(vessel) \Rightarrow \frac{d_{min}}{o.d.} \Rightarrow d_{min}$$

5

where + infers a spatial relation which would be calculated using suitable ray tracing software to give values for vessel and assembly dimensions.

Specifically, knowing dimensions and refractive indices, ray tracing, for example using Zemax software, may be used to produce diagrams allowing relationships between dimensions such as  $d_{min} / o.d.$  to be deduced. A schematic diagram showing the cross section of a cylindrical vessel and the surface of the detector is shown in Figure 5: symbols, given here in brackets, are for the inner diameter (i.d.), the outer diameter (o.d.), and the outer wall to detector distance ( $d$ ). Preferably for example for a sample vessel having circular outer and inner wall cross-section and constructed of quartz or silica, and for solvent of refractive index in the range 1.325 – 1.345 (encompassing for example typical reversed phase HPLC solvents methanol, water and acetonitrile), the minimum distance for spatial separation of the core and wall beams using collimated light incident on the vessel may be calculated from values given in Table 1. For example, for a ratio  $i.d./o.d. = 0.50$ , the minimum value of  $d/o.d.$  to achieve beam separation (defined as > 90% separation of core and wall beam fluxes) is 0.5. For a capillary with actual dimensions corresponding to this criterion, e.g. i.d. 100  $\mu m$  and o.d. 194  $\mu m$ , the minimum value of  $d/o.d.$  is 0.5 and thus the minimum value of  $d$  is 100  $\mu m$ .

25

The advantage of having as high an  $i.d./o.d.$  as possible is to have a low value of  $d/o.d.$ , in order to minimise detector cross-talk between adjacent vessels.

Values of  $d/o.d.$  greater than the minimum are permissible, but the greater the value, the more the constraints on how close the vessels can be positioned.

There are situations in which no separation of the core and wall beams is possible. For example, for a cylindrical vessel, this occurs in two generic cases. Firstly, if the refractive index of the material in the core is too low, for example air in a silica or glass vessel (Figure 6). Secondly, if the ratio  $i.d./o.d.$  is too low, for example water in a silica or glass vessel of  $i.d./o.d.$  ratio 0.2 (Figure 8). The actual dimensions for the capillary in Figure 8 are  $i.d.$  75  $\mu m$  and  $o.d.$  364  $\mu m$ , a capillary type widely used in capillary electrophoresis. Figure 7 shows that for the same  $i.d.$  but a smaller  $o.d.$ , 194  $\mu m$ , beam separation is readily achieved.

Consideration of the optical properties of filled cylindrical vessels show that the constraints of refractive index and  $i.d./o.d.$  are interdependent, emphasising that for each vessel and contents type, each case should be considered on its merits.

In the case where the refractive index of the vessel contents is higher than that of the vessel walls, no beam separation is possible except at distances unreasonably close to the vessel outer wall.

The vessel may be associated with additional optical components in the emergent light path, to focus or otherwise manipulate one or both of the spatially separated beam types.

The array may comprise fixed or variable spacers between each sample vessel for adjusting spacing of emergent beams B in a sequence for vessels 1 2 3 etc, as shown in Figure A, having wall  $w$  and core  $c$ , for example wherein each beam corresponds to an array detection location:



B1w B1c B1w B2w B2c B2w B3w B3c B3w...

If desired, adjacent wall beams may be coincident:

5

B1w B1c B1w/B2w B2c B2w/B3w B3c B3w/...

Other out of step arrangements are possible but may require more complex coupling and reading of detector location.

10

Spacers may comprise elongate filters designed to screen all or part of a wall light path, or a filter to screen part of the vessel wall thereby confining the wall light paths, in both cases for minimising intercapillary stray light and cross talk.

15

A spacer may therefore be of any suitable material for combined spacing and filtration, optionally also serving as support means for the at least one sample vessel, and is of suitable opaque material such as for example an opaque glass filled polymer.

20

Sample vessels may be comprised of any transparent polymer, glass, quartz, silica, e.g. fused silica or other material, preferably optical grade. Optical grade polymers include the classes of siloxanes such as polydimethylsiloxane (PDMS), amorphous polycycloolefins based on norbornene, and polymethylmethacrylate PMMA, polycarbonate, and other transparent flexible polymers and fluoropolymers. Flexible transparent polymers are commercially available as transparent flexible tubing such as polyetherimide such as Ultem, polypropylene, fluoropolymers including the transparent PCTFE, ECTFE, ETFE, PTFE, PFA, FEP or PVDF resins, preferably the fluoropolymer Tygon chemfluor 367 and the like.

30

The vessel wall may be transparent in part or whole and is preferably of the same material throughout.

5 A capillary as hereinbefore defined may comprise any extruded capillary or microfabricated capillary or channel or other parallel elongate closed conduit means. A capillary may be flexible or rigid and may be straight or curved along all or part of its length.

10 Capillary arrays and microfabricated channel arrays are commercially available. Capillary arrays are typically manufactured by drawing or extrusion, creating a void circular cross-section core of high uniformity dimensions. Microfabricated arrays are typically manufactured by injection moulding from a tool, creating a void square or rectangular cross-section channel, which is then optionally sealed with a cover layer, and offers the advantage of absolute  
15 reproducibility of highly precise channels, and freedom of channel design.

A sample vessel may comprise part of an array of any number of vessels, commercially available arrays include 8 to 1536 vessels, preferably 8 to 520 capillaries or 96 to 1536 wells, for example 8, 12, 16, 24, 32, 48 or 96  
20 capillaries or 96, 384 or 1536 wells.

The vessel may comprise part of an array of a greater number of vessels which may be available in the future.

25 Micro fabricated arrays fabricated in layered planar manner, constructing interfacing elements of a device in sequential planes, are gaining acceptance and widespread use. They have numerous advantages in accuracy, reproducibility, ease and flexibility of manufacture.

Vessels may have any desired separation, suitably are fused or adjacent or are spaced apart. A lower separation increases packing density but a higher separation reduces intervessel interference, in particular optical interference. It is a particular advantage of the invention that intervessel spacing may be used.

5 This is not possible in the embodiment of Yeung *et al* above, for example which needs minimal vessel separation to minimise stray light.

The vessel may be of suitable length and depth according to the desired use. Preferably for capillaries or channels length is in the range 2 cm - 2 m for  
10 example in the range 2.5 - 6 cm for microfabricated channels or 6 - 100 cm length for capillaries, more preferably 10 to 60 cm. Greater length allows application of higher voltage in capillary electrophoresis and improved separation. For microtitre plate well, preferable inter-vessel centre to centre spacings are compatible with standard microtitre plate formats, such as 2.25,  
15 4.5 and 9 mm.

Preferably a vessel is of 3  $\mu\text{m}$  to 20 mm in depth or internal diameter, and 4  $\mu\text{m}$  to 30 mm in external diameter, more preferably 9  $\mu\text{m}$  - 3 mm in depth or internal diameter and 10  $\mu\text{m}$  to 3.5 mm in external diameter, more preferably  
20 10-380  $\mu\text{m}$ , most preferably less than or equal to 200  $\mu\text{m}$  in depth or internal diameter or external diameter. A vessel wall is importantly of suitable thickness for the optical properties of the invention. This is particularly relevant for vessels of small internal diameters. Accordingly vessel internal diameter or "bore" may be selected and vessel wall material selected, and  
25 suitable outer diameter determined accordingly to give the required optical properties. For silica capillaries with internal diameter (hereinafter i.d.) in the range 20 to 250  $\mu\text{m}$ , for example 20, 25, 50, 75 or 100  $\mu\text{m}$ , external diameters (hereinafter o.d.) is preferably in the range 100 to 380  $\mu\text{m}$ , for example 150, 200 or 360  $\mu\text{m}$ . For example a vessel may be of 75-100  $\mu\text{m}$  i.d. and 194  $\mu\text{m}$

o.d. or 180  $\mu\text{m}$  i.d. and 364  $\mu\text{m}$  o.d.. It is important to note that for a vessel with 75  $\mu\text{m}$  i.d. and 364  $\mu\text{m}$  o.d., as widely used in capillary electrophoresis, no separation of core and wall beams is possible when working with aqueous solutions. For silica capillaries, thickness is suitably in the range 30 – 500  $\mu\text{m}$ ,  
5 for example 30 – 150  $\mu\text{m}$ : vessels of low i.d. preferably have low wall thickness, to give a minimum i.d. to o.d. ratio of 2 - 4 for example 0.25.

When working with larger diameter reaction vessels, similar constraints apply, but normally the i.d./o.d. ratio falls in the range giving suitable beam  
10 separation. For example, a glass reaction vessel having an i.d. of 20 mm and an o.d. of 30 mm has an i.d./o.d. ratio equal to 0.67, which permits beam separation with all common solvents (see Table 1). For a polycarbonate reaction vessel and water as solvent, for an i.d. of 0.33 cm, an o.d. of 1.0 cm would be suitable, but an o.d. of 1.5 cm would be unsuitable. For a  
15 representative fluoropolymer tubing, Tygon chemfluor 367, with i.d. 1/16" (1.6 mm) and o.d. 1/8" (3.2 mm), the i.d./o.d. ratio is 0.50 and beam separation with solvent water is achieved for all values of the ratio  $d/\text{o.d.}$  greater than 0.4, i.e.  $d > 1/20"$  (1.3 mm). However, when working with hexane as a solvent in  
20 such tubing, the refractive index of the vessel contents is greater than that of the walls (values of refractive indices are given in footnote to Table 1), and no beam separation is possible other than at distances unreasonably close to the vessel outer wall.

The sample vessel may be void or packed, for example may comprise  
25 stationary phase or may be coated or otherwise configured with suitable materials as known in the art for example in HPLC. Suitably packing if present is of corresponding refractive index to bulk phase sample or to solvent comprised in sample to be detected.

Preferably the vessel comprises internals and components characteristic of columns or capillaries present in pressure driven or electrical driven separations including HPLC (for pressure driven) or capillary electrochromatography (CEC) (electrically driven equivalent of HPLC, separating by binding or partition coefficient, using eg hydrophobic stationary phases), micellar electrokinetic chromatography, and capillary electrophoresis (CE) including the focusing and concentrating techniques of isoelectric focusing (IEF separating by isoelectric point independent of size and shape of molecules), isotachopheresis (ITP), capillary zone electrophoresis (CZE separating by charge to size ratio) and dynamic field gradient focussing (DFGF, where a constant hydrodynamic force is opposed by a gradient in the electric field, which allows charged molecules to focus in order of their apparent electrophoretic mobilities and selective concentration of analytes e.g. proteins – see “Digitally controlled electrophoretic focusing” Huang and Cornelius, Anal. Chem., 1999, 71, 1628-1632).

The separation between a sample vessel and the detector,  $d$ , is suitably such as to facilitate coupling of spatially separated light paths to the detector locations. Suitably the separation is a function of the vessel o.d. and of the degree of separation of light paths, and is preferably given by the ratio  $d/\text{o.d.}$  is less than 10, for example is in the range 0.5 – 5, preferably 0.5 – 1. In a particular advantage the optical assembly of the invention allows an extremely compact structure when working with capillaries in which separation  $d$  is of the order of 50 – 360  $\mu\text{m}$ , for example 200  $\mu\text{m}$ . This is particularly advantageous since the lesser the value  $d$  the more compact and robust is the assembly and the more intense are the transmitted light beams at the detector. The separation  $d$  may be adapted to couple spatially separated light paths in sequence as

hereinbefore defined, with or without intervening optical components and preferably without intervening optical components.

There are a number of commercially available array detecting systems, including for example the commonly used photodiodes and more recently available charge coupled devices (CCDs) and active pixel sensors (APSs) eg complementary metal oxide semiconductor (CMOS).

Preferably therefore an array detector according to the invention comprises a solid state sensing device, more preferably a CCD, CID or a CMOS APS.

A detection zone may be of any desired area size and is suitably of zone dimensions substantially equal to the vessel or array cross section in a plane perpendicular to the light path, corresponding to one to one image. A detection zone may comprise one or a plurality of array detectors.

Smaller zone size increases noise and reduces sensitivity yet can be provided at lower cost. Preferably the apparatus comprises lowest noise and highest sensitivity CCDs in a relatively small area device, such as a 1024 x 256 pixel CCD (MAT CCD30-11).

A CCD for use in the apparatus of the invention may have 22 to 5000 or more pixels in either dimension, preferably 256, 512, 770, 1152, 2048 or 4096 pixels, of pixel size 7 to 35  $\mu\text{m}$ , preferably 20 to 30  $\mu\text{m}$ , more preferably 22 to 30  $\mu\text{m}$ . Preferably the CCD comprises 3 to 28, for example 10 pixels per capillary or 30 to 2500 for example 100 pixels per well. Pixels outside the imaging area are preferably not digitised to reduce readout time.

Commercially available CCDs may include a stud, for protection of the CCD surface which is usually recessed in the CCD support package and to conserve image quality. Preferably the stud comprises a coating to absorb incident light and reemit at a different wavelength, to convert UV to visible light, to allow  
5 detection by the CCD. A coating is for example a phosphor coating. The phosphor coating may be applied directly to the stud or to a cover slip interleaved between the stud and capillary, facilitating changing phosphor as needed, by replacing the cover slip without need to replace the stud.

10 Each camera is interfaced to control means, preferably a processing control means providing a suitable pixel readout rate, suitably of the order of MHz, preferably greater than 4 or 5 MHz.

Preferably the processing means is programmed for selection of on-chip  
15 charge binning procedures, to increase signal current (photoelectrons per second) and selection of area of interest for read out. Additionally the processing means controls camera readout and collects, stores and analyses data.

20 In the case of an assembly comprising a conduit sample vessel intended for dynamic sample detection, preferably the apparatus operates with real-time signal processing for optimum peak detection and parameterisation/characterisation, and potential for automatic system management including closed-loop feedback control of the apparatus and  
25 systems. For example, feedback could include stopping or slowing the flow following initial observation in the detection window, to allow sample to reside in the detector window and give longer-times for data acquisition and enhanced signal to noise or to facilitate detection along the length of a vessel.

Flow velocity may be controlled by adjustment of electric field (as in capillary electrophoresis) or by adjustment of pressure (as in liquid chromatography), or by a combination of the two. For flow driven by centrifugal forces, flow velocity control is carried out by adjustment of the angular velocity.

5

Suitably the assembly comprises means to detect presence of sample in a detection window, and feedback control means for turning off the voltage when it is detected as having migrated to the centre of the window (see Figure 13). Feedback control means suitably includes means for monitoring the subsequent broadening of the sample peak due to diffusion as a function of time, and for analysis of the change in peak variance with time, and determining the diffusion coefficient, enabling the hydrodynamic radius of the analyte to be deduced, and means for combining with the mobility, obtained from the time taken to reach the window under a given field strength, enabling the charge on the analyte to be deduced. The control means is able to operate with any starting peak shape, since convolution of the peak with a Gaussian enables the Gaussian component of the peak broadening to be extracted. Data quality obtained with the assembly of the invention is such that diffusion coefficients could be measured with good precision in less than 3 minutes.

10 This assembly could be used to measure diffusion coefficients, size and charges of both small molecules and large molecules, including proteins, DNA, and polysaccharides, and offer a simpler alternative to analytical ultracentrifuge methods.

25 Alternatively closed loop feedback could include means such as peak recognition and decision making software for instructing a switching valve and controlling switching times to enable fraction collection, or to direct a fraction to a mass spectrometer, e.g. via an electrospray interface, or to a NMR



spectrometer. Means for observing the flow stream both before and after the valve enables the quality of analyte switching and efficiency of the switching means to be monitored. A schematic example of closed-loop feedback control is given in Figure 14. Preferably the assembly positions the capillary in two  
5 separate light paths and to generate two sets of spatially separated transmitted light paths coupled to two detectors or detector zones with the switching valve therebetween whereby after the appropriate switch the eluent is monitored again in a second pass of the detector, so that the efficiency of the switching process can be monitored. An alternative is to have more of the outputs of the  
10 switching valve passing the detector for visualisation.

Closed loop feedback may also include controlling velocity of samples in multiple vessels, for example in a capillary array, to co-ordinate exit times, in sequence or, for combining samples from different capillaries into a common  
15 exit means, simultaneously. Velocity may be controlled by controlling voltage or pressure, for example pumping flow rate, and may be operated with switching devices. Velocity may enable stopping samples flow at desired time to coincide with an event which is to be performed on the sample or is to take place in the sample. Controlled exit may be for subsequent fraction collection  
20 or analysis, for example for interfacing the output of a capillary bundle to a mass spectrometer by electro-spray, or to an NMR spectrometer or the like.

Preferably controlled loop feedback is provided by creating a potential difference across the length of the capillary and/or varying the applied voltage  
25 to control migration of sample, including slowing or stopping to improve signal/noise ratio and including timing sample migration to achieve a desired time of arrival of sample at a point to switch into a sample collection means such as mass spectrometer. The system may operate with a pressure difference and pumping, electrical field driver, column switching or the like. Preferably

- therefore a capillary comprises electrodes, valves or pressure regulators at the ends thereof or along the length thereof about the detection zone or each detection zone together with circuitry to control electrodes or to facilitate pumping control. In the case of voltage controlled migration, preferably a sample vessel is connected to a buffer supply and electric field is arranged such that buffer supply and sample introduction is at the high potential end of the capillary, where high may be either positive or negative with respect to ground.
- 10 In a further aspect of the invention there is provided an optical assembly module for use with a column or capillary separating device as known in the art, wherein the vessel is a capillary or column comprising interfacing means at one end for inserting into the outlet of a column or capillary separating device and optionally comprising interfacing means enabling insertion into the inlet of an analysing means at the other end or comprising interface means at both ends for insertion along the length of a capillary or column. A module for insertion along the length of a column or capillary typically has a column or capillary section of matching i.d and o.d as the separating device or interfacing means allowing a smooth flow transition.
- 20 In a further aspect of the invention there is provided an optical assembly clip-on device adapted to locate about a section of a capillary or column which is of suitable i.d, o.d and refractive index as hereinbefore defined comprising means to locate about the capillary or column of a separation device.
- 25 Optionally the capillary or column has its outlet inserted into the mass spectrometer, in which case the clip-on is located as close to the mass spectrometer as possible. In the case of a clip-on, the capillary or column of the separation device may be stripped of any surface coating to facilitate the operation of the method of the invention, whereby the stripped capillary or

column, such as a capillary electrophoresis or microbore HPLC section, provides the sample vessel of the assembly.

5 In a further aspect of the invention there is provided an apparatus for chemical reaction or synthesis and analysis or for sample separation or transport wherein the apparatus comprises the optical assembly as hereinbefore defined. The chemical reaction vessel itself could be cylindrical and the reaction monitored in batch flow mode as a function of time, and feedback control used to halt reaction – e.g by admixture of a quenching reagent, by change of  
10 temperature, or by exporting the vessel contents. Alternatively the reaction vessel could be tubular and used in continuous flow mode. The apparatus may comprise a plurality of means for introducing one or more reagents to the at least one sample vessel together with means for regulating reaction conditions to form a desired chemical synthetic reaction within the at least one sample  
15 vessel; or may include means for inlet and outlet of sample in dynamic fashion into the at least one sample vessel together with means for applying a pressure difference or potential difference across the ends of the vessel and means for supplying separation mediums such as buffer in order to perform separations within the at least one sample vessels; or may include a separation means such  
20 as a chromatography column as known in the art having outlet interfaced with an inlet end of the at least one sample vessel as hereinbefore defined for dynamic analysis of separated sample.

25 In a further aspect of the invention there is provided a method for detection of light transmitted through at least one sample contained within the core of at least one sample vessel of an optical assembly as hereinbefore defined, comprising illuminating the vessel with a substantially collimated light source or sources and detecting transmitted light in a detector, wherein transmitted light is spatially separated into at least two light paths, a wall path which has

passed through the vessel walls only, spatially separated from a core path which has passed through the walls and core, wherein the spatially separated light beams are coupled to individual detection locations on the array detector. Suitably the method comprises any features or embodiments corresponding to  
5 apparatus features and embodiments outlined above.

Preferably the method is a method for detecting light from samples in sample analysis for example for high throughput screening (HTS) or profiling or assays, such as enzyme assays; and uses thereof in the pharmaceutical,  
10 biomedical and bioscience, healthcare, agrochemical, veterinary, industrial, environmental or materials or like fields, for detection, analysis, characterisation and quantification or the like of samples contained in a vessel, and optionally further collecting separated components thereof; in particular in combinatorial chemistry; in metabolomics, proteomics or genomics, assay and  
15 high throughput analysis applications, typically high sensitivity analyses, separation and/or quantification studies and for sample separation for example chromatography or electrophoresis, in particular column chromatography, capillary electrophoresis with real time or post separation analysis, in hospital or surgery blood tests and other assays, in industrial quality control, in  
20 environmental pesticide level monitoring and the like.

The method may be a method for detecting light from a static or dynamic sample. Typically a static sample is contained in a closed ended sample vessel as hereinbefore defined, more typically in a vessel in the form of a cell or well  
25 which may be one of a plurality of vessels for example in a microtitre plate or a well plate or sample plate as hereinbefore defined. Samples derived from enzyme assay or other multiple sample analysis may be in this form for detection.

In one embodiment the method is a method for single capillary or multicapillary absorbance detection, comprising drawing solvent then sample into the capillary(s), by capillary action, pressure, pipetting or the like, conducting detection of difference in transmittance of sample and solvent, and  
5 disposing of or blowing sample back to the source. This method is useful in bioscience for making absorbance measurements on small sample volumes of microlitres or less. Enzyme assays may be conducted with one or two streams entering the vessel and detecting a time-dependent change, normally in profiling, for enzyme assay.

10

Typically dynamic samples are electrically or pressure driven and are present in an open ended conduit type vessel as hereinbefore defined, such as a capillary having inlet and outlet ends for flow of sample through the capillary, the capillary may be a single capillary or part of a capillary array as  
15 hereinbefore defined. Samples derived from high throughput screening or from the separation or transport techniques may be provided in this manner for detection, of which samples derived from separation techniques may be provided for separation within the capillary with simultaneous detection of light transmission, or may be separated in a separation method such as column  
20 chromatography, and the separated sample flow from the column coupled directly into a capillary for detection of light transmission.

Preferably the method for detecting a dynamic sample is a method for column or capillary separation as known in the art, suitably selected from pressure  
25 driven or electrical driven separations including HPLC (for pressure driven) or capillary electrochromatography (CEC) (electrically driven equivalent of HPLC, separating by binding or partition coefficient, using eg hydrophobic stationary phases), micellar electrokinetic chromatography, and capillary electrophoresis (CE) including the focusing and concentrating techniques of

isoelectric focusing (IEF separating by isoelectric point independent of size and shape of molecules), isotachopheresis (ITP), capillary zone electrophoresis (CZE separating by charge to size ratio) and dynamic field gradient focussing (DFGF, where a constant hydrodynamic force is opposed by a gradient in the electric field, which allows charged molecules to focus in order of their apparent electrophoretic mobilities and selective concentration of analytes e.g. proteins – see “Digitally controlled electrophoretic focusing” Huang and Cornelius, Anal. Chem., 1999, 71, 1628-1632). Other electrically driven techniques are known or may be developed in future.

10

A method which is a method for electrophoretic separation of molecules is carried out with an assembly, module or clip-on in a capillary or channel as hereinbefore defined which is connected to a buffer supply. An electric field in the range of kilovolts is applied across both ends of the capillary or channel to cause the molecules to migrate. Samples are typically introduced at a high potential end and, under the influence of the electric field, move toward a low potential end of the channel. Absorbance analysis may be conducted along the length of the capillary or channel or near the outlet allowing observing an entire process taking place in the length of the capillary or channel or the result thereof.

20

Another use of dynamic detection is in measuring refractive index change. By analysis of the illumination pattern of the core beam at high spatial resolution perpendicular to the capillary axis, the detector has the ability to monitor refractive index change in the solvent in the capillary. This would allow distinction between two solvents, and by extension the ability to directly monitor the mobile phase composition during a gradient elution separation in dual solvent mixtures. If necessary, magnification in the direction perpendicular to the capillary axis could be used to increase the resolution in

25

terms of mobile phase composition. This would be of benefit in HPLC. Since solvent refractive index may be temperature dependent, application of a heat pulse providing a temperature rise up-stream of the detector could be used to determine the mobile phase velocity in capillary HPLC.

5 Another use of multicapillary absorbance detection is for rapid measurement of  $pK_a$ . Here aliquots of the sample solution are mixed into a set of buffer solutions covering a range of pH values, typically spanning the range 2-12, and all mixtures are then drawn up into separate capillaries in the sequence  
10 buffer then mixture of buffer plus sample. By taking measurements at one or more wavelengths where acid and base forms have different absorbance, results from all capillaries of absorbance as a function of pH may be processed to determine  $pK_a$  values. Using suitable non- or weakly-absorbing inorganic buffers, this is applicable for organic or biological compounds containing all  
15 common titratable functional groups, including carboxyl and amine groups, and at concentrations down to 100 micromolar. This is of benefit in for example the pharmaceutical industry and for high throughput screening.

The invention has particular use in relation to samples of small molecules of  
20 MW of the order 15 – 500, but may also be used in relation to samples of larger molecules such as polymers, proteins, DNA and other biomolecules of MW of the order 500 to  $10^6$ . The invention is of particular advantage in one embodiment due to its small size. This may be employed to advantage in hospitals and the like for sample analysis, without the need for clinical  
25 biochemical laboratories, for example as a colour assay. Blood tests may be conducted on blood samples which are currently spun to separate red blood cells and plasma in a laboratory. The assembly of the invention may be used to detect red blood and plasma, either before or after centrifugation, for example by adding a reagent to the plasma region and observing the reaction.

In an alternative embodiment multiple wavelength detection allows detection at a range of wavelengths along the length of a capillary or channel.

- 5 Preferably the method is a method enabling or allowing some transformation or event to occur in a vessel and imaging the event. Imaging may be conducted at the end of the transformation or event or throughout. Imaging throughout an event requires timing to coincide with migration of sample in the vessel, preferably using controlled loop feedback as hereinbefore defined  
10 to stop the sample migration in the vessel at desired location or interval for imaging.

For example the method may be a method for observing a chemical reaction for biomedical, bioscience, healthcare, agrochemical, veterinary,  
15 pharmaceutical, industrial or environmental purpose, wherein multiple detection may be performed on the inlet and outlet and in the waste to ensure that all of the reaction product has been collected. The reaction may be conducted in the vessel in the form of capillary which may be curved, allowing ease of detection of multiple positions using a common light source  
20 and detector.

In an alternative embodiment the method comprises detecting sample from pharmaceutical studies, in the form of analyte in solvent such as dimethylsulfoxide (DMSO), stored in microtitre plates, as is common in  
25 pharmaceutical practice. The method of the invention may be performed on samples either in the microplate array in situ, as a vessel array as hereinbefore defined or following drawing up portions into one or more capillaries, as a single capillary or capillary array. Use of a short path length of less than 9 mm, preferably of the order of 300  $\mu\text{m}$  or less, allows UV absorbance  
30 detection without total absorption of light by the DMSO solvent.



In an alternative embodiment the method is a method for measuring physico-chemical properties for example partition coefficients, comprising placing sample of analyte in a first solvent in the vessel, together with a second immiscible solvent, for example water and octanol respectively, and observing the analyte moving between the two immiscible phases. In a particular advantage the method of the invention also enables imaging of the solvent phases whereby their interface is also visible.

10 In an alternative embodiment the method may be a method for detection of light from a plurality of sample vessels for high throughput analysis of different samples in each vessel, for example for comparative analysis thereof or may be a high loading method for detecting in each vessel the same samples from a high volume, high flow or otherwise bulk upstream process, intended  
15 for combining a desired component from each sample. A high loading method may comprise introducing the output from a single HPLC for example having flow rate exceeding that possible in a single capillary, but suitable for introducing into a capillary array which may then function effectively as a single detector. For example the method may comprise detecting analytes  
20 present in sample in or exiting a microbore liquid chromatography column and the column may be of diameter in the micron range up to millimetre range. High loading in a plurality or array of vessels achieves higher resolution in separation and potentially higher sensitivity in detection than operation on a large scale in a single vessel from a single large bore separation channel.  
25 Moreover a shorter path length is possible in an array of capillaries than is possible in a standard HPLC cell and this allows operation at a lower wavelength as hereinbefore defined.

A method for detection in DFGF or multiple detection method preferably  
30 employs feedback control as hereinbefore defined.

Preferably the method comprises illuminating the at least one sample vessel with collimated light comprising a single or a plurality of wavelengths selected in the range as hereinbefore defined. In a particular advantage  
5 illumination is with a collimated light source of a single wavelength at any given time, thereby simplifying readout of optical detection results.

A sample as hereinbefore defined may comprise any sample of one or more small or large molecules present in liquid or gel phase suitably in solution with  
10 liquid phase solvent or cosolvent such as an inert or non reactive liquid. Solvent or gel may have refractive index in the range as hereinbefore defined. Suitably however these samples are characterised by a refractive index of lower than but of similar order to that of the sample vessel walls, whereby the sample provides a generally convergent light path. Preferably therefore the  
15 sample comprises a solution or a suspension of molecules to be detected in a solution or suspending medium selected from water, alcohols, acetonitrile, hexane, dichloromethane, acetone, DMSO and other common solvents and cosolvents and mixtures thereof; or the sample may be provided in the form of a gel for example uncrosslinked polymer solutions such as cellulose  
20 derivatives (e.g. hydroxypropyl cellulose) and synthetic polymers (e.g. polyethylene oxide).

Preferably the method of the invention comprises selecting a sample for analysis, determining individual wavelengths at which absorption by desired  
25 sample components is strongest, checking refractive index of the sample in order to select a suitable sample vessel which when containing the sample and when illuminated will generate spatially separated beams as hereinbefore defined or selecting a suitable combination of optical components, filters and the like and a suitable vessel to detect an array separation to couple spatially  
30 separated beams to independent locations on the detector array.

Sample may be introduced into the at least one sample vessel as hereinbefore defined in known manner, for example by injection, loop injection, pipette, hydrostatic, electrokinetic or like injection techniques and may be removed  
5 from the vessel in known manner such as injection, electrospray or other interface for discard or to a further vessel for storage or to a down stream identification means such as mass spectrometer.

Detected light is coupled to individual detection locations on the array detector  
10 as hereinbefore defined. The at least one sample vessel as hereinbefore defined is coupled to a plurality of detector locations in manner that core detector locations correspond to the core light path from the at least one vessel and peripheral detector locations correspond to the peripheral wall point(s) from the vessel. Preferably the method comprises imaging the transmitted light  
15 detected by the detection means, for example in the form of a CCD image as known in the art. Preferably the method also comprises referencing the light detected by the detection means by means of exposure referencing wherein the ratio of the core beam intensity to the wall beam intensity gives a value for the sample intensity at each location with elimination of excess or flicker noise  
20 due to light source fluctuation.

Accordingly therefore the method comprises coupling the at least one sample vessel to at least three detector locations, preferably 3 to 25 detector locations for a sample vessel of the order of microns diameter wherein the locations  
25 may be apportioned for example 1:1:1 – 5:15:5 or 8:9:8 depending on the relative wall and core beam width; and for a sample vessel of the order of cm in an amount of 30 to 2500 pixels per sample vessel for example in the ratio 5:20:5 or 10:10:10 to 500:1500:500 or 800:900:800 depending on the relative wall and core beam width. The method may include pixel summing or the like  
30 for enhanced signal strength and noise reduction as known in the art.

Preferably the method includes subsequently measuring the amount of absorption of light by species in the sample vessel which indicates the amount of absorbing species in manner as known in the art and comprising measuring  
5 the intensity of light in the absence and presence of the sample. In a particular advantage measurement according to the invention is simply by measuring intensity of light in a wall beam and a core beam. The logarithm of the ratio, taken in conjunction with values measured in the absence of sample, provides the absorbance according to the Beer-Lambert Law.

10 Absorbance may be imaged, for example as a CCD snapshot. Preferably however the method is a method for snapshot detection whereby detection is recorded in a plurality of finite exposures, for example five exposures per second, and exposures are super imposed, directly in the case of a static  
15 example or with time displacement in the case of a dynamic sample. Accordingly an individual image reveals limited information and therefore the detection array preferably provides raw data which is compiled and converted to graphical display for example in the form of an electropherogram.

20 In a further aspect of the invention there is provided the use of the optical assembly, method and apparatus as hereinbefore defined in sample analysis for example for high throughput screening (HTS), for example in an array as hereinbefore defined, or profiling or assays, such as enzyme assays; and uses thereof in the pharmaceutical, biomedical and bioscience, healthcare,  
25 agrochemical, veterinary, materials, industrial, environmental, and like fields, for detection, analysis, characterisation and quantification or the like of samples contained in a vessel, and optionally further collecting separated components thereof; in particular in combinatorial chemistry; in metabolomics, proteomics or genomics, assay and high throughput analysis  
30 applications, typically high sensitivity analyses, separation and/or

quantification studies and for sample separation for example chromatography or electrophoresis, in particular column chromatography, capillary electrophoresis with real time or post separation analysis; in hospital or surgery blood tests and other assays, in industrial quality control, in  
5 environmental pesticide level monitoring and the like.

The invention is now illustrated in non limiting manner with respect to the following examples and Figures wherein

10 Figure A shows elevations of capillary array type vessels and detection means of an optical assembly of the invention

Figure 1 shows a schematic diagram of apparatus of the invention for parallel capillary absorbance detection

Figure 2 shows a collimated illumination of rectangular CCD area (26.6 x 6.7  
15 mm) using light output from a 1 mm diameter fused-silica optical fibre (N.A. = 0.22) using a cylindrical and spherical fused-silica lens element

Figure 3 shows the CCD and vessel arrangement of the optical assembly of the invention

Figure 4 shows part of one CCD snapshot showing ~ 3mm of 4 capillaries  
20 (100  $\mu\text{m}$  i.d., 194  $\mu\text{m}$  o.d.); the total area imaged is 6.7 x 26.6 mm. The contents of the capillaries are 1. Air, 2. Water, 3 and 4. ink solution

Figure 5 shows light beam ray tracing diagram according to the invention showing light path through a water filled capillary, 100  $\mu\text{m}$  i.d., 194  $\mu\text{m}$  o.d.. The dark rays represent the light passing through the water at the capillary  
25 centre and the light rays show the light that passes only through the capillary walls. The dashed line shows the approximate position of the fibre optic stud surface

Figure 6 shows light beam tracings not according to the invention showing light path through an air filled capillary, 100  $\mu\text{m}$  i.d., 194  $\mu\text{m}$  o.d.

Figure 7 shows light beam tracings according to the invention showing light path through a water filled capillary, 75  $\mu\text{m}$  i.d., 194  $\mu\text{m}$  o.d.

Figure 8 shows light beam tracings not according to the invention showing light path through a water filled capillary, 75  $\mu\text{m}$  i.d., 364  $\mu\text{m}$  o.d.

- 5 Figure 9 shows electropherograms of  $\sim 16$  nL 100 microM 4-nitrophenol injected into each of four parallel 100  $\mu\text{m}$  i.d. capillaries. Capillary length: 500 mm total, 300 to the detector. Separation voltage: 5000 V. Buffer:sodium phosphate pH 7.5 (15 mM sodium)

- Figure 10 shows electropherograms of 100 microM 4-nitrophenol after  
10 correction for cross-talk between capillaries

Figure 11 shows electropherograms of  $\sim 16$  nL 1 microM 4-nitrophenol injected into each capillary

Figure 12 shows electropherogram generated by taking the average of the four traces shown in Figure 11

- 15 Figure 13 shows peak imaging and variance for a sample of rhodamine 700 injected onto a capillary and migrated by CE to the detection zone which is imaged by laser induced fluorescence with a CCD. The voltage is turned off (at  $\Delta t=0$ ) and the peak broadening due to diffusion is monitored for 1800 s (top). The change in peak variance is plotted against time (bottom)

- 20 Figure 14 shows a schematic of a possible arrangement for closed loop feedback control. The output from a liquid chromatography system is monitored during a first pass of the area detector. Peak recognition and decision making software can instruct the switching valve to direct the appropriate fraction for collection or for example to a mass spectrometer  
25 interface. After the appropriate switch the eluent is monitored again in a second pass of the detector so that the efficiency of the switching process can be monitored. An alternative would be to have more of the outputs from the switching valve passing the detector for visualisation

- Figure 15 shows an illumination pattern perpendicular to the capillary axis created by light passing through the core of a 75  $\mu\text{m}$  i.d. 194  $\mu\text{m}$  o.d. capillary positioned 260  $\mu\text{m}$  from the detection surface. Plots are shown for the capillary containing water and acetonitrile (at 20 °C, sodium D line); the difference in the illumination pattern would allow the direct determination of the mobile phase composition during a gradient elution separation. Acetonitrile at 44 °C has the same refractive index as water does at 20 °C; the same approach could be used to determine the mobile phase velocity by applying a heat pulse upstream of the detector.
- Figure 16 is a diagram showing an optical assembly clip-on device of the invention showing the approximate dimensions for absorbance detection according to the invention, such as CE or absorbance. A module device of the invention would differ by comprising a capillary with interfacing means to insert into a capillary eg from microLC or into mass spectrometer.

15

### Example 1

- The experimental setup is shown in Figure 1. The output from a 75 W xenon lamp is launched into a single 1 mm diameter fused silica fibre. The light output from the fibre is shaped and collimated using cylindrical and spherical fused silica lens elements (Figure 2) to illuminate the rectangular area of the CCD. The CCD chip used is EEV CCD 30-11 and is thermostatted and controlled by a system designed and built by York Electronics Centre; it has 1024 by 256 active pixels, each 26  $\mu\text{m}$  square, with a total active area of 6.7 x 26.6 mm. The CCD chip has a fibre optic stud (faceplate) that protects the CCD surface. The fibre optic stud is not UV transparent, so a UV phosphor is coated onto the surface of stud to make the detector sensitive to a wide wavelength range from NIR to below 200 nm. The charge accumulated on the CCD is read out in a series of snapshots; to

prevent image smearing a light chopper ensures that the CCD is not illuminated during the readout period. An exposure rate of 5 Hz is used with a 50% duty cycle (100 ms exposure and 100 ms readout time). An image of  $1024 \times 256$  pixels with 14 bit digitisation is obtained from each snapshot.

5

An ideal arrangement of the capillaries could be to align them parallel to the short axis of the CCD at a spacing of  $260 \mu\text{m}$  (10 pixels per capillary). This arrangement would allow up to 102 capillaries, which is ideal to accommodate the number used if sampling from a standard 96 well plate.

10 The spacing means a gap of  $66 \mu\text{m}$  between each capillary, this would allow more reference light reaching the CCD than in the current arrangement with the capillaries more tightly packed. Better exposure referencing and lower inter capillary cross talk should result from this arrangement.

#### 15 Capillary imaging

In the demonstration experiment four fused silica capillaries ( $100 \mu\text{m}$  i.d.,  $194 \mu\text{m}$  o.d. 500 mm long) were placed side by side, approximately  $200 \mu\text{m}$  above the CCD and parallel to the long axis of the CCD as shown in Figures 1 and 3. The portion of the capillaries imaged was a section 273.4 to 300.0 mm from the inlet end. Figure 4 shows a portion of one snapshot taken with the four capillaries filled with air, water and the last two with an ink solution. Excellent referencing is seen for the assembly without any lenses or other optics. It can be seen from the comparison between capillaries 1 and 2 that the collimated light that passes through the capillary core is  
20 convergent when the capillary is filled with water, producing a line that is brighter than the background. Figures 5 and 6 show in detail how light passes through the water and air filled capillaries; they show also that in the case of the filled capillary, there is good separation on the CCD between the  
25 light passing through the capillary core and that only passing through the



capillary walls. This is confirmed in Figure 4 where a high contrast is observed between the images of the water and ink filled capillaries. It is important to use capillaries with a small o.d.; Figure 7 shows that good results would be obtained using capillaries with the same o.d. of 194  $\mu\text{m}$  as used here but with the more commonly used 75  $\mu\text{m}$  i.d. However, the 364  $\mu\text{m}$  o.d. capillary normally used in capillary electrophoresis would not be suitable; Figure 8 shows that the larger radius at the air/fused-silica interface does not adequately focus the light having passed through the capillary core to spatially separate it from the light having passed only through the capillary walls. During an experiment the image from the whole CCD was read into the computer for each exposure; for this experiment an area of  $32 \times 1024$  pixels contained the image of the four capillaries; the remainder was discarded to conserve computer memory. The data was further reduced by adding together the pixel values in groups of four down the capillary length to give a total of  $32 \times 256$  effective pixels for each snapshot; each effective pixel has 16 bit resolution and dimensions of  $26 \times 104 \mu\text{m}$ .

#### Exposure referencing

Fluctuations in exposure times and in the light source intensity that is in excess of shot noise need to be accounted for in order to get the best possible performance from the detector. This is usually achieved by using a double beam arrangement, where a portion of the light from the source that does not pass through the sample is monitored and used as a reference. The ratio of this reference and the light that does pass through the sample is used to calculate the absorbance. In this experiment the light that strikes the CCD having passed only through the capillary walls is used as the reference. The electrophoresis of 4-nitrophenol in its ionic form was used to test the performance of the detection system. An optical filter with a centre wavelength of 405 nm and bandpass of 10 nm was placed at the input to the

fibre optic to match the absorbance wavelength of 4-nitrophenol at pH 7.5 (absorbance coefficient,  $\epsilon_{405}=1700 \text{ m}^2 \cdot \text{mol}^{-1}$ ). To establish which of the image pixels were to be used as 'reference pixels' and which to use as 'sample pixels' snapshots with the capillaries filled with water were compared with those with the capillaries containing a 1 mM solution of 4-nitrophenol. The average pathlength is  $\pi d/4 = 79 \text{ }\mu\text{m}$ ; this corresponds to an absorbance of 0.13 AU for this solution. The pixels that showed a reduction in signal in the presence of the 4-nitrophenol solution that corresponded to an absorbance of  $<0.02$  were used as reference pixels, those with  $> 0.1$  were used as sample pixels.

#### Capillary electrophoresis and data processing

A series of parallel capillary electrophoresis experiments were carried out using a pH 7.5, sodium phosphate buffer (15 mM sodium) on dilutions of a 4-nitrophenol solution made up in buffer. Injections were performed inserting the inlet end of all the capillaries into the sample solution that was held at 2 cm above the level of the buffer in the outlet vial for 15 s. The volume injected into each capillary by siphoning should be approximately 16 nL. A voltage of +5 kV was applied to the inlet vial and the electrophoresis was carried out; electroosmotic flow ensured that the analyte moved towards the grounded cathode at the outlet. The snapshot data was accumulated in the computer RAM during the experiment and saved to disk at the end of a run.

The raw data collected during an experiment was first corrected for fixed pattern noise as described in detail in "A charge coupled device array detector for single-wavelength and multi-wavelength ultraviolet absorbance in capillary electrophoresis", Bergstrom and Goodall, Pokric and Allinson, Anal. Chem. 1999, 71, 4376-4384, and then processed to produce a set of

electropherograms, one for each capillary. This ensures that high spatial resolution is maintained, limited only by the dimensions of the effective pixels used, 106  $\mu\text{m}$  in this case.

5 Figure 9 shows the four electropherograms obtained using a sample solution of 100  $\mu\text{M}$ . It is clear from the dips in the base line at times corresponding to peaks in adjacent capillaries that there is cross talk between capillaries. This is mainly caused by some light passing through the sample being used as part of the reference, and to a lesser extent there is some light that after  
10 passing through the sample in one capillary lands on a sample pixel of an adjacent capillary. The extent of both of these effects has been measured by filling each capillary in turn with the sample solution. It has been assumed that the level of cross talk scales linearly with absorbance and the correction based on the measurement at this single sample concentration has been  
15 applied to all subsequent experiments. The appropriate correction is readily made as is demonstrated by Figure 10.

#### Noise performance

Figure 11 shows the four electropherograms obtained by injecting a solution  
20 of 1  $\mu\text{M}$  4-nitrophenol. The peak heights in Figure 11 correspond to a concentration of  $\sim 0.6 \mu\text{M}$ , the limit of detection is calculated to be 0.22  $\mu\text{M}$  based on three times the RMS baseline noise of 9.4  $\mu\text{AU}$  (1 s risetime). The theoretical shot noise limited baseline noise level was calculated by generating simulated data sets based on the average exposure patterns and  
25 levels found in the experiment and assuming a pixel full well capacity of  $5 \times 10^5$  electrons. These generated snapshot data sets were processed identically to the experimental data sets; the RMS shot noise level was found to be 9.0  $\mu\text{AU}$ . This is very close to the observed value and indicates that the detector is shot noise limited.

The CCD used in this experiment is large enough to accommodate over 30 capillaries aligned as the four are here. The sensitivity of detection for each of these capillaries would be the same as found in this study (i.e.  $\sim 9 \mu\text{AU}$  RMS noise with a rise-time of 1 s). Alternatively over 120 capillaries could be accommodated if they were aligned parallel to the short dimension of the CCD; this would result in a reduction in the signal integration time for each capillary by a factor of four and therefore an increase in noise level by a factor of  $\sqrt{4} = 2$ . Capillary electrophoresis with arrays of capillaries obviously has application for high throughput analysis as the number of separations that can be carried out simultaneously simply scales with the size of the array. However, if the same sample is simultaneously injected into all the capillaries in the array, as done in this experiment, it is a means to increase sample loading and therefore dynamic range and concentration sensitivity. If all of the electropherograms are combined by taking the arithmetic average after compensation for the slight differences in analyte velocities between capillaries, then an increase in signal to noise of  $\sqrt{N}$  is achieved, where  $N$  is the number of capillaries. Splitting a large sample load into many capillaries reduces the problems associated with overloading which include poor peak shape induced by electromigration dispersion and large injection lengths, and nonlinear detector response at high absorbances of highly abundant components. Figure 12 shows the result of averaging the four electropherograms of Figure 11. The RMS baseline noise level is  $4.7 \mu\text{AU}$ , a reduction by a factor of 2 of the individual traces, this is the improvement expected for 4 capillaries.

The noise performance measured by combining the signal from four capillaries is still at the shot noise limit and is better than the performance achieved previously in Bergström et al above, where it was suggested that

fluctuations in the spatial distribution of the lamp discharge, which is imaged on the fibre bundle input, would result in fluctuations in the spatial distribution of the CCD illumination. This would result in a noise level that is in excess of the shot noise because separate areas of the CCD monitor the signal and reference levels. Using a single optical fibre instead of the fibre bundle used previously should to a large degree scramble any spatial inhomogeneities of the lamp discharge. Scaling up the experiment to 30 parallel capillaries should give a combined RMS baseline noise level of 1.7  $\mu$ AU, corresponding to an on column 4-nitrophenol concentration LOD of 40 nM.

When the analyte concentration is low relative to the concentration of background electrolyte then it should only be the length of the injection plug and analyte diffusion that contribute significantly to the measured peak width, assuming that the spatial resolution of the detector is high. The peak variance caused by analyte diffusion can be calculated,  $\sigma^2 = 2Dt = 1.2 \times 10^{-6} \text{ m}^2$ , where  $D$  is the diffusion coefficient ( $8.1 \times 10^{-10} \text{ m}^2 \text{ s}^{-1}$  for 4-nitrophenol) and  $t$  is time. The contribution to the peak variance from the length of the plug of sample injected is given by  $l_i^2/12 = 0.4 \times 10^{-6} \text{ m}^2$  (where  $l_i$  is the injection length of 2.0 mm). These two contributions give a total standard deviation,  $\sigma$ , of 1.3 mm; dividing by the analyte velocity gives  $\sigma = 3.2 \text{ s}$  in units of time. This compares well with a standard deviation of 3.1 s measured by fitting a Gaussian function to the peak in Figure 12. This is experimental evidence that the detection method of imaging a 26.6 mm capillary section and of subsequently combining parallel electropherograms does not degrade separation efficiency.

### Example 2

**Table 1.** Table showing, for vessel with circular outer and inner cross sections, minimum values of ratio of the outer wall to detector distance  $d$  and the outer diameter of the vessel o.d. ( $d/o.d.$ ) in order to obtain spatial separation between core and wall beams. Values are shown as a function of ratio of inner and outer diameters of the vessel (i.d./o.d.) for a range of solvents and vessel materials. Entries x indicate no spatial separation possible.

	i.d./o.d. 0.20	i.d./o.d. 0.25	i.d./o.d. 0.33	i.d./o.d. 0.50
Water/silica	x	2.0	1.0	0.5
Hexane/silica	1.6	1.0	0.6	0.4
Dichloromethane/silica	0.6	0.5	0.4	0.2
Water/polycarbonate	x	x	2.1	0.5
Water/flexible clear tubing (Tygon chemfluor 367)	0.5	0.5	0.5	0.4

Values of refractive indices used in ray tracing analysis are: silica (1.458), water (1.333), hexane (1.375), dichloromethane (1.424), polycarbonate (1.585), Tygon chemfluor 367 (1.34). Other common reversed phase HPLC solvents, often used in admixture with water, are methanol (1.329) and acetonitrile (1.344): these and their mixtures will give similar values of  $d/o.d.$  to water for the various vessel types. Hexane may be grouped with two other common normal phase HPLC solvents of comparable refractive index, 2-propanol (1.378) and ethyl acetate (1.372). The method used in constructing this Table is also effective for determining values for other solvents such as DMSO (1.479).

From the Table, for a known o.d. capillary the required i.d. can be determined from one of the possibilities to give a value of  $d/o.d.$  and thereby value of  $d$ , as described in the description.

### Example 3 – Feedback Control

An example of feedback control is the use in a CE experiment for stopping the sample in the detection window, by turning off the voltage when it is detected as having migrated to the centre of the window (see Figure 13). After stopping, the subsequent broadening of the sample peak due to diffusion is monitored as a function of time. Analysis of the change in peak variance with time enables the diffusion coefficient to be determined. The hydrodynamic radius of the sample molecule may then be calculated using Stokes law. Combination of the diffusion coefficient with the mobility, obtained from the time taken to reach the window under a given field strength, enables the charge on the analyte to be deduced. Any starting peak shape is acceptable, since convolution of the peak with a Gaussian enables the Gaussian component of the peak broadening to be extracted. Whilst the example shows peak broadening measured over a period of 30 minutes, data quality is such that diffusion coefficients could be measured with good precision in less than 3 minutes.

A schematic example of closed-loop feedback control is given in Figure 14. Here the output from an LC system is monitored during a first pass of the area detector. Peak recognition and decision making software is used to instruct the switching valve to direct the appropriate fraction for collection or for example to a mass spectrometer interface. After the appropriate switch the eluent is monitored again in a second pass of the detector, so that the efficiency of the switching process can be monitored. An alternative is to have more of the outputs of the switching valve passing the detector for visualisation.

### Example 4 - Uses

The detection method of the invention is used in measuring refractive index change. By analysis of the illumination pattern of the core beam at high spatial resolution perpendicular to the capillary axis, the detector has the ability to monitor refractive index change in the solvent in the capillary. Figure 15 shows, for a 75  $\mu\text{m}$  i.d., 194 mm o.d. capillary positioned 260  $\mu\text{m}$  from the detector surface, the change in profile of the core beam on changing from water (refractive index 1.333) to acetonitrile (refractive index 1.344). With a pixel size of 10  $\mu\text{m}$ , this would allow distinction between the two illumination profiles, and by extension the ability to directly monitor the mobile phase composition during a gradient elution separation in water-acetonitrile mixtures. If necessary, magnification in the direction perpendicular to the capillary axis could be used to increase the resolution in terms of mobile phase composition. This would be of benefit in HPLC. Since acetonitrile at 44  $^{\circ}\text{C}$  has the same refractive index as water does at 20  $^{\circ}\text{C}$ , application of a heat pulse providing a 25  $^{\circ}\text{C}$  temperature rise up-stream of the detector could be used to determine the mobile phase velocity in capillary HPLC.

Another use of multicapillary absorbance detection is for rapid measurement of  $\text{pK}_{\text{a}}$ . Here aliquots of the sample solution are mixed into a set of buffer solutions covering a range of pH values, typically spanning the range 2-12, and all mixtures are then drawn up into separate capillaries in the sequence buffer then mixture of buffer plus sample. By taking measurements at one or more wavelengths where acid and base forms have different absorbance, results from all capillaries of absorbance as a function of pH may be processed to determine  $\text{pK}_{\text{a}}$  values. Using suitable non- or weakly-absorbing inorganic buffers, this is applicable for organic or biological compounds containing all common titratable functional groups, including carboxyl and amine groups, and at concentrations down to 100 micromolar. This is of benefit in for example the pharmaceutical industry and for high throughput screening.



### CLAIMS

1. An optical assembly comprising a light source, at least one sample vessel and a detector, the at least one vessel being positioned in a light path or  
5 paths created between the source and the detector in manner to enable transmission of light through the vessel wherein the light source is adapted to provide a beam of substantially collimated light, the detector comprises a plurality of detector locations and the vessel comprises a wall and core of relative shape and dimensions adapted to contain a sample for detection and  
10 to define at least two spatially separated transmitted light paths, a first wall path which enters and exits the vessel walls only, spatially separated from a second core path which enters and exits the vessel walls and additionally the vessel core, wherein the spatially separated wall and core paths are coupled to individual detector locations on the detector.
- 15
2. Optical assembly of Claim 1 wherein the detector is an array detector.
3. Optical assembly of any of Claims 1 to 2 wherein the assembly defines a central core path and two peripheral wall paths either side thereof or an  
20 annular wall path thereabout.
4. Optical assembly of any of Claims 2 to 3 wherein core and wall path beams are spatially close, preferably adjacent, on the array detector, facilitating direct referencing as the ratio of the core beam to the wall beam.
- 25
5. Optical assembly of any of Claims 1 to 4 wherein the light source comprises at least one wavelength of light that is absorbed by one or more absorbing species, the absorbance of which is to be detected.

6. Optical assembly of any of Claims 1 to 5 wherein the light source output is coupled from an optical fibre.
7. Optical assembly of any of Claims 1 to 6 wherein light is of wavelength  
5 in the range 160 to 1200 nm, preferably 180 or 190 to 1200 nm, corresponding to UV, UV-vis to near infra red (NIR).
8. Optical assembly of any of Claims 1 to 7 wherein the at least one  
10 sample vessel in the assembly of the invention comprises a cell or conduit which may be closed or open ended and closed or open based and topped, intended for static or dynamic sample detection.
9. Optical assembly of any of Claims 1 to 8 wherein the sample vessel is a  
15 single cell or one of a plurality of cells in an array; or is a single capillary or one of a plurality of capillaries in a microcapillary array or a microfabricated channel array.
10. Optical assembly of any of Claims 1 to 9 wherein  
20 illumination:detection magnification is in the range 0.8 – 1.5:1.
11. Optical assembly of any of Claims 1 to 10 which is characterised by  
respective outer and inner diameter of a sample vessel, and by respective  
refractive indices of vessel walls and of sample, wherein refractive index of  
the vessel wall is greater than that of the bulk phase of any sample comprised  
25 in the core whereby the wall and core paths are spatially separated.
12. Optical assembly of any of Claims 1 to 11 in which the sample vessel  
comprises an outer and inner wall which are of similar cross-section or shape  
or different for which a cross-section in a plane including the transmission

light path is independently square or rectangular, curved circular or angular or a combination thereof and is symmetrical or asymmetrical.

13. Optical assembly of any of Claims 1 to 12 wherein outer and inner  
5 vessel walls are of coaxial circular cross-section thereby defining an annular wall having outer and inner diameters such that refraction and spatial separation of core and wall beams is achieved.

14. Optical assembly of Claim 13 characterised by i.d.(vessel) in the range  
10 3 micron to 20 mm, o.d.(vessel) in the range 4 micron to 30mm, refractive index (vessel) in the range 1.3 - < 1.6, refractive index (sample) in the range 1.3 to in excess of 1.5, ratio  $d/o.d.$  is 0.5 to 10 and  $d$  is in the range 20 micron to 300 mm.

15. Optical assembly of any of Claims 1 to 14 wherein a vessel is  
15 composed of transparent polymer, glass, quartz, silica, e.g. fused silica or other optical grade material.

16. Optical assembly of any of Claims 1 to 15 wherein the vessel wall is  
20 optically transparent in part or whole and is preferably of the same material throughout.

17. Optical assembly of any of Claims 1 to 16 wherein the vessel i.d./o.d.  
ratio falls in a range giving suitable beam separation with all common  
25 solvents, for example

$$\frac{i.d.}{o.d.} + r.i.(solvent) + r.i.(vessel) \Rightarrow \frac{d_{min}}{o.d.} \Rightarrow d_{min}$$

where + infers a spatial relation which would be calculated using suitable ray tracing software to give values for vessel and assembly dimensions.

18. Optical assembly of any of Claims 14 to 17 wherein  $d/o.d.$  is in the  
5 range 0.5 – 5 and  $d$  is of the order of 50 – 360 micron, for example 200 micron.
19. Optical assembly of any of Claims 1 to 19 wherein an array detector  
comprises a solid state sensing device.
- 10 20. Optical assembly of any of Claims 1 to 19 wherein an array detector  
comprises a CCD including a surface stud comprising a coating to absorb  
incident light and reemit at a different wavelength, to convert UV to visible  
light, to allow detection by the CCD, wherein the coating is applied directly to  
15 the stud or to a cover slip interleaved between the stud and vessel, facilitating  
recoating as needed, by replacing the cover slip without need to replace the  
stud.
21. Optical assembly of any of Claims 1 to 20 which comprises means for  
20 real-time signal processing for optimum peak detection and  
parameterisation/characterisation, and means for automatic system  
management including closed-loop feedback control of the apparatus and  
systems.
- 25 22. Optical assembly of any of Claims 1 to 21 in which closed-loop  
feedback control means includes means for stopping or slowing the flow  
following initial observation in the detection means to allow sample to reside  
in the detector window and give longer times for data acquisition and

enhanced signal to noise or to enable fraction collection, or to direct a fraction to an analysis means such as mass spectrometer.

23. Method for detection of light transmitted through at least one sample  
5 contained within the core of at least one sample vessel of an optical assembly  
as hereinbefore defined in any of Claims 1 to 22, comprising illuminating the  
vessel with a substantially collimated light source or sources and detecting  
transmitted light in a detector, wherein transmitted light is spatially separated  
into at least two light paths, a wall path which has passed through the vessel  
10 walls only, spatially separated from a core path which has passed through the  
walls and core, wherein the spatially separated light beams are coupled to  
individual detection locations on the array detector.

24. Method of Claim 23 which is a method for detecting light from samples  
15 in sample analysis for example for high throughput screening (HTS) or  
profiling or assays, such as enzyme assays; and uses thereof in the  
pharmaceutical, biomedical and bioscience, agrochemical, veterinary,  
materials and like fields, for detection, analysis, characterisation and  
quantification or the like of samples contained in a vessel, and optionally  
20 further collecting separated components thereof; in particular in combinatorial  
chemistry; in metabolomics, proteomics or genomics, assay and high  
throughput analysis applications, typically high sensitivity analyses, separation  
and/or quantification studies and for sample separation for example  
chromatography or electrophoresis, in particular column chromatography,  
25 capillary electrophoresis with real time or post separation analysis.

25. Method of any of Claims 23 to 24 which is a method for detecting light  
from a static or dynamic sample.

26. Method of any of Claims 23 to 25 wherein a sample is any vessel contents which comprise a single or multiple components, wherein multiple components are present as a homogeneous or heterogeneous mixture, and optionally undergo migration with time ie may be a plurality of liquid phase components optionally including a dissolved phase component; or include one or a plurality of analytes which it is desired to detect in one or a plurality of solvents or like bulk phase sample component, for example in the course of a chemical reaction generating or consuming a species as analyte..
27. Method of any of Claims 23 to 26 which is a method selected from pressure driven or electrical driven separations column or capillary separations including high pressure liquid chromatography (HPLC) or capillary electrochromatography (CEC), micellar electrokinetic chromatography, and capillary electrophoresis (CE) including the focusing and concentrating techniques of isoelectric focusing (IEF), isotachophoresis (ITP), capillary zone electrophoresis (CZE) and dynamic field gradient focussing (DFGF).
28. Method of any of Claims 23 to 27 in which a sample is of one or more small or large molecules present in liquid or gel phase suitably in solution with liquid phase solvent or cosolvent such as an inert or non reactive liquid characterised by a refractive index of lower than but of similar order to that of the sample vessel walls.
29. Method of any of Claims 23 to 28 which additionally comprises selecting a sample for analysis, determining individual wavelengths at which absorption by desired sample components is strongest, checking refractive index of the sample in order to select a suitable sample vessel which when containing the sample and when illuminated will generate spatially separated beams as hereinbefore defined or selecting a suitable combination of optical

components, filters and the like and a suitable vessel to detect an array separation to couple spatially separated beams to independent locations on the detector array.

- 5     30. Method of any of Claims 23 to 29 in which sample is introduced into the at least one sample vessel by injection, loop injection, pipette, hydrostatic, or electrokinetic injection and is removed from the vessel by injection, electrospray or other interface for discard or to a further vessel for storage or to a down stream identification means.

10

31. Method of any of Claims 23 to 30 which comprises imaging the transmitted light detected by the detection means, for example in the form of a CCD image.

- 15     32. Method of any of Claims 23 to 31 which comprises referencing the light detected by the detection means by means of exposure referencing wherein the ratio of the core beam intensity to the wall beam intensity gives a value for the sample intensity at each location with elimination of excess or flicker noise due to light source fluctuation.

20

33. Method of any of Claims 23 to 32 which includes subsequently measuring the amount of absorption of light by species in the sample vessel which indicates the amount of absorbing species by measuring the intensity of light in the absence and presence of the sample, or by measuring intensity of  
25     light in a wall beam and a core beam, wherein the logarithm of the ratio, taken in conjunction with values measured in the absence of sample, provides the absorbance according to the Beer-Lambert Law.

34. Module optical assembly of any of Claims 23 to 33 for use with a column or capillary separating device as known in the art, wherein the vessel is a capillary or column comprising interfacing means at one end for inserting into the outlet of a column or capillary separating device or along the length thereof, the capillary or column and optionally comprising interfacing means enabling insertion into the inlet of an analysing means at the other end.
35. Clip-on device for an optical assembly of any of Claims 23 to 33 comprising means for locating about a section of a capillary or column separating device which is of suitable i.d, o.d. and refractive index as hereinbefore defined and is stripped of any surface coating to facilitate the operation of the method of the invention, whereby the stripped capillary or column provides the sample vessel of the assembly.
36. Apparatus for chemical reaction or synthesis and analysis or for sample separation or transport wherein the apparatus comprises the optical assembly of any of Claims 23 to 35 as hereinbefore defined in which the chemical reaction vessel itself is cylindrical and the reaction monitored in batch flow mode as a function of time, and feedback control used to halt reaction – e.g by admixture of a quenching reagent, by change of temperature, or by exporting the vessel contents - or in which the reaction vessel is tubular and used in continuous flow mode.
37. Use of the optical assembly, method and apparatus, module or clip-on as hereinbefore defined in any of Claims 1 to 36 in sample analysis for example for high throughput screening (HTS) or profiling or assays, such as enzyme assays; and uses thereof in the pharmaceutical, biomedical and bioscience, agrochemical, veterinary, materials and like fields, for detection, analysis, characterisation and quantification or the like of samples contained in



a vessel, and optionally further collecting separated components thereof; in particular in combinatorial chemistry; in metabolomics, proteomics or genomics, assay and high throughput analysis applications, typically high sensitivity analyses, separation and/or quantification studies and for sample  
5 separation for example chromatography or electrophoresis, in particular column chromatography, capillary electrophoresis with real time or post separation analysis.

38. Assembly, method, module, clip-on device or use thereof substantially  
10 as herein described or illustrated in the description, the examples and/or the figures.

**AMENDED CLAIMS**

**[Received by the International Bureau on 03 February 2004 (03.02.04):  
original claims 1-38 replaced by amended claims 1-44; (9 pages)]**

1. An optical assembly comprising a light source, at least one sample vessel and a detector, the at least one vessel being positioned in a light path or  
5 paths created between the source and the detector in manner to enable transmission of light through the vessel wherein the light source is adapted to provide a beam of substantially collimated light, the detector comprises a plurality of detector locations and the vessel comprises a wall and core of relative shape and dimensions adapted to contain a sample for detection and  
10 to define at least two spatially separated transmitted light paths, a first wall path which enters and exits the vessel walls only, spatially separated from a second core path which enters and exits the vessel walls and additionally the vessel core, wherein the spatially separated wall and core paths are coupled to individual detector locations on the detector, and the detector is an array  
15 detector.
2. Optical assembly of Claim 1 wherein the assembly defines a central core path and two peripheral wall paths either side thereof or an annular wall path thereabout.  
20
3. Optical assembly of any of Claims 1 and 2 wherein core and wall path beams are spatially close, preferably adjacent, on the array detector, facilitating direct referencing as the ratio of the core beam to the wall beam.
- 25 4. Optical assembly of any of Claims 1 to 3 wherein the light source comprises at least one wavelength of light that is absorbed by one or more absorbing species, the absorbance of which is to be detected.

5. Optical assembly of any of Claims 1 to 4 wherein the light source output is coupled from an optical fibre.
6. Optical assembly of any of Claims 1 to 5 wherein light is of wavelength  
5 in the range 160 to 1200 nm, preferably 180 or 190 to 1200 nm, corresponding to UV, UV-vis to near infra red (NIR).
7. Optical assembly of any of Claims 1 to 6 wherein the at least one sample vessel in the assembly of the invention comprises a cell or conduit  
10 which may be closed or open ended and closed or open based and topped, intended for static or dynamic sample detection.
8. Optical assembly of any of Claims 1 to 7 wherein the sample vessel is a single cell or one of a plurality of cells in an array; or is a single capillary or  
15 one of a plurality of capillaries in a microcapillary array or a microfabricated channel array.
9. Optical assembly of any of Claims 1 to 8 wherein illumination:detection magnification is in the range 0.8 – 1.5:1.  
20
10. Optical assembly of any of Claims 1 to 9 which is characterised by respective outer and inner diameter of a sample vessel, and by respective refractive indices of vessel walls and of sample, wherein refractive index of the vessel wall is greater than that of the bulk phase of any sample comprised  
25 in the core whereby the wall and core paths are spatially separated.
11. Optical assembly of any of Claims 1 to 10 in which the sample vessel comprises an outer and inner wall which are of similar cross-section or shape or different for which a cross-section in a plane including the transmission

light path is independently square or rectangular, curved circular or angular or a combination thereof and is symmetrical or asymmetrical.

12. Optical assembly of any of Claims 1 to 11 wherein outer and inner  
5 vessel walls are of coaxial circular cross-section thereby defining an annular wall having outer and inner diameters such that refraction and spatial separation of core and wall beams is achieved.
13. Optical assembly of Claim 12 characterised by i.d.(vessel) in the range  
10 3 micron to 20 mm, o.d.(vessel) in the range 4 micron to 30mm, refractive index (vessel) in the range  $1.3 < 1.6$ , refractive index (sample) in the range 1.3 to in excess of 1.5, ratio  $d/o.d.$  is 0.5 to 10 and  $d$  is in the range 20 micron to 300 mm.
14. Optical assembly of any of Claims 1 to 13 wherein a vessel is  
15 composed of transparent polymer, glass, quartz, silica, fused silica or other optical grade material.
15. Optical assembly of any of Claims 1 to 14 wherein the vessel wall is  
20 optically transparent in part or whole.
16. Optical assembly of any of Claims 1 to 15 wherein the vessel wall is of the same material throughout.
17. Optical assembly of any of Claims 1 to 16 wherein the vessel i.d./o.d. ratio falls in a range giving suitable beam separation with all common solvents.
- 25

18. Optical assembly of any of Claims 1 to 16 wherein the vessel i.d./o.d. is given by

$$\frac{i.d.}{o.d.} + r.i.(solvent) + r.i.(vessel) \Rightarrow \frac{d_{min}}{o.d.} \Rightarrow d_{min}$$

5 where + infers a spatial relation which would be calculated using suitable ray tracing software to give values for vessel and assembly dimensions.

19. Optical assembly of any of Claims 13 to 18 wherein  $d/o.d.$  is in the range 0.5 – 5 and  $d$  is of the order of 50 – 360 micron.

10

20. Optical assembly of any of Claims 13 to 19 wherein  $d$  is of the order of 200 micron.

15 21. Optical assembly of any of Claims 1 to 20 wherein an array detector comprises a solid state sensing device.

22. Optical assembly of any of Claims 1 to 21 wherein an array detector comprises a CCD including a surface stud comprising a coating to absorb incident light and reemit at a different wavelength, to convert UV to visible  
20 light, to allow detection by the CCD, wherein the coating is applied directly to the stud or to a cover slip interleaved between the stud and vessel, facilitating recoating as needed, by replacing the cover slip without need to replace the stud.

25 23. Optical assembly of any of Claims 1 to 22 which comprises means for real-time signal processing for optimum peak detection and parameterisation/characterisation, and means for automatic system

management including closed-loop feedback control of the apparatus and systems.

24. Optical assembly of any of Claims 1 to 23 in which closed-loop  
5 feedback control means includes means for stopping or slowing the flow  
following initial observation in the detection means to allow sample to reside  
in the detector window and give longer times for data acquisition and  
enhanced signal to noise or to enable fraction collection, or to direct a fraction  
to an analysis means.

10

25. Method for detection of light transmitted through at least one sample  
contained within the core of at least one sample vessel of an optical assembly  
as hereinbefore defined in any of Claims 1 to 24, comprising illuminating the  
vessel with a substantially collimated light source or sources and detecting  
15 transmitted light in an array detector, wherein transmitted light is spatially  
separated into at least two light paths, a wall path which has passed through  
the vessel walls only, spatially separated from a core path which has passed  
through the walls and core, wherein the spatially separated light beams are  
coupled to individual detection locations on the array detector.

20

26. Method of any of Claims 25 to 25 which is a method for detecting light  
from a static or dynamic sample.

27. Method of any of Claims 25 to 26 wherein a sample is any vessel  
25 contents which comprise a single or multiple components, wherein multiple  
components are present as a homogeneous or heterogeneous mixture, and  
optionally undergo migration with time.

28. Method of Claim 27 wherein a sample is a plurality of liquid phase components optionally including a dissolved phase component; or includes one or a plurality of analytes which it is desired to detect in one or a plurality of solvents or like bulk phase sample component,

5

29. Method of Claim 28 wherein a sample includes one or a plurality of analytes which it is desired to detect in the course of a chemical reaction generating or consuming a species as analyte.

10 30. Method of any of Claims 25 to 29 which is a method selected from pressure driven or electrical driven separations column or capillary separations including high pressure liquid chromatography (HPLC) or capillary electrochromatography (CEC), micellar electrokinetic chromatography, and  
15 techniques of isoelectric focusing (IEF), isotachophoresis (ITP), capillary zone electrophoresis (CZE) and dynamic field gradient focussing (DFGF).

31. Method of any of Claims 25 to 30 in which a sample is of one or more small or large molecules present in liquid or gel phase suitably in solution with  
20 liquid phase solvent or cosolvent characterised by a refractive index of lower than but of similar order to that of the sample vessel walls.

32. Method of any of Claims 25 to 31 which additionally comprises selecting a sample for analysis, determining individual wavelengths at which  
25 absorption by desired sample components is strongest, checking refractive index of the sample in order to select a suitable sample vessel which when containing the sample and when illuminated will generate spatially separated beams as hereinbefore defined or selecting a suitable combination of optical components and filters and a suitable vessel to detect an array separation to

couple spatially separated beams to independent locations on the detector array.

33. Method of any of Claims 25 to 32 in which sample is introduced into  
5 the at least one sample vessel by injection, loop injection, pipette, hydrostatic, or electrokinetic injection and is removed from the vessel by injection, electrospray or interface for discard or to a further vessel for storage or to a down stream identification means.

10 34. Method of any of Claims 25 to 33 which comprises imaging the transmitted light detected by the detection means

35. Method of Claim 34 wherein imaging is in the form of a CCD image.

15 36. Method of any of Claims 25 to 35 which comprises referencing the light detected by the detection means by means of exposure referencing wherein the ratio of the core beam intensity to the wall beam intensity gives a value for the sample intensity at each location with elimination of excess or flicker noise due to light source fluctuation.

20

37. Method of any of Claims 25 to 36 which includes subsequently measuring the amount of absorption of light by species in the sample vessel which indicates the amount of absorbing species by measuring the intensity of light in the absence and presence of the sample, or by measuring intensity of  
25 light in a wall beam and a core beam, wherein the logarithm of the ratio, taken in conjunction with values measured in the absence of sample, provides the absorbance according to the Beer-Lambert Law.



38. Module optical assembly of any of Claims 1 to 24 for use with a column or capillary separating device as known in the art, wherein the vessel is a capillary or column comprising interfacing means at one end for inserting into the outlet of a column or capillary separating device or along the length thereof, the capillary or column optionally comprising interfacing means enabling insertion into the inlet of an analysing means at the other end.

39. Clip-on device optical assembly of any of Claims 1 to 24 comprising means for locating about a section of a capillary or column separating device which is of suitable i.d, o.d. and refractive index as hereinbefore defined and is stripped of any surface coating to facilitate the operation of the method of the invention, whereby the stripped capillary or column provides the sample vessel of the assembly.

40. Apparatus for chemical reaction or synthesis and analysis or for sample separation or transport wherein the apparatus comprises the optical assembly of any of Claims 1 to 24 as hereinbefore defined in which the chemical reaction vessel itself is cylindrical and the reaction monitored in batch flow mode as a function of time, and feedback control used to halt reaction or in which the reaction vessel is tubular and used in continuous flow mode.

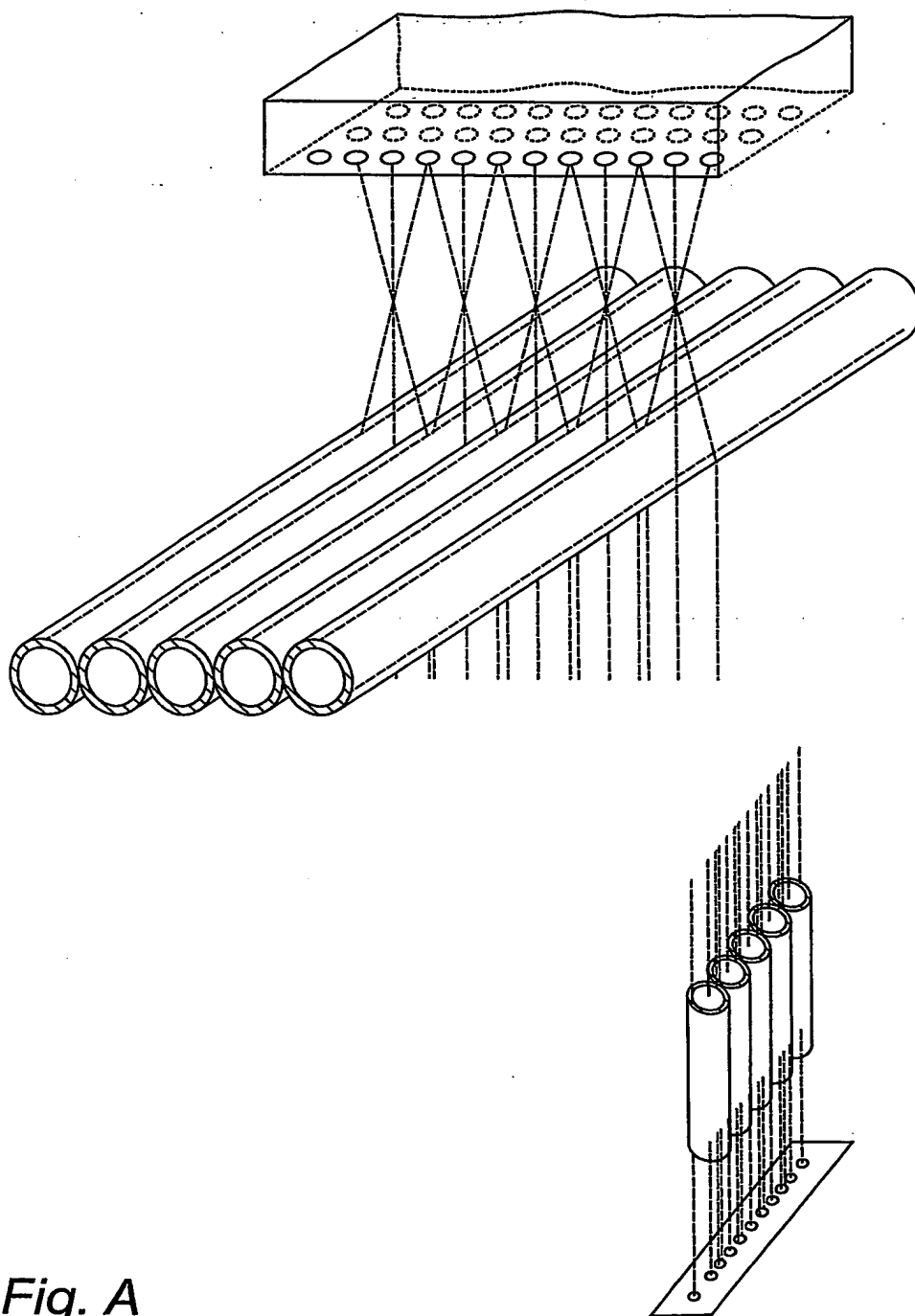
41. Use of the optical assembly, method and apparatus, module or clip-on as hereinbefore defined in any of Claims 1 to 40 in the pharmaceutical, biomedical and bioscience, agrochemical, veterinary and materials fields, for detection, analysis, characterisation and quantification of samples contained in a vessel, and optionally further collecting separated components thereof.

42. Use according to Claim 41 in combinatorial chemistry; in metabolomics, proteomics or genomics, assay and high throughput analysis applications, or for sample separation by chromatography or electrophoresis.

5 43. Use according to Claim 41 or 42 in enzyme assays, high sensitivity analyses, column chromatography, capillary electrophoresis with real time or post separation analysis.

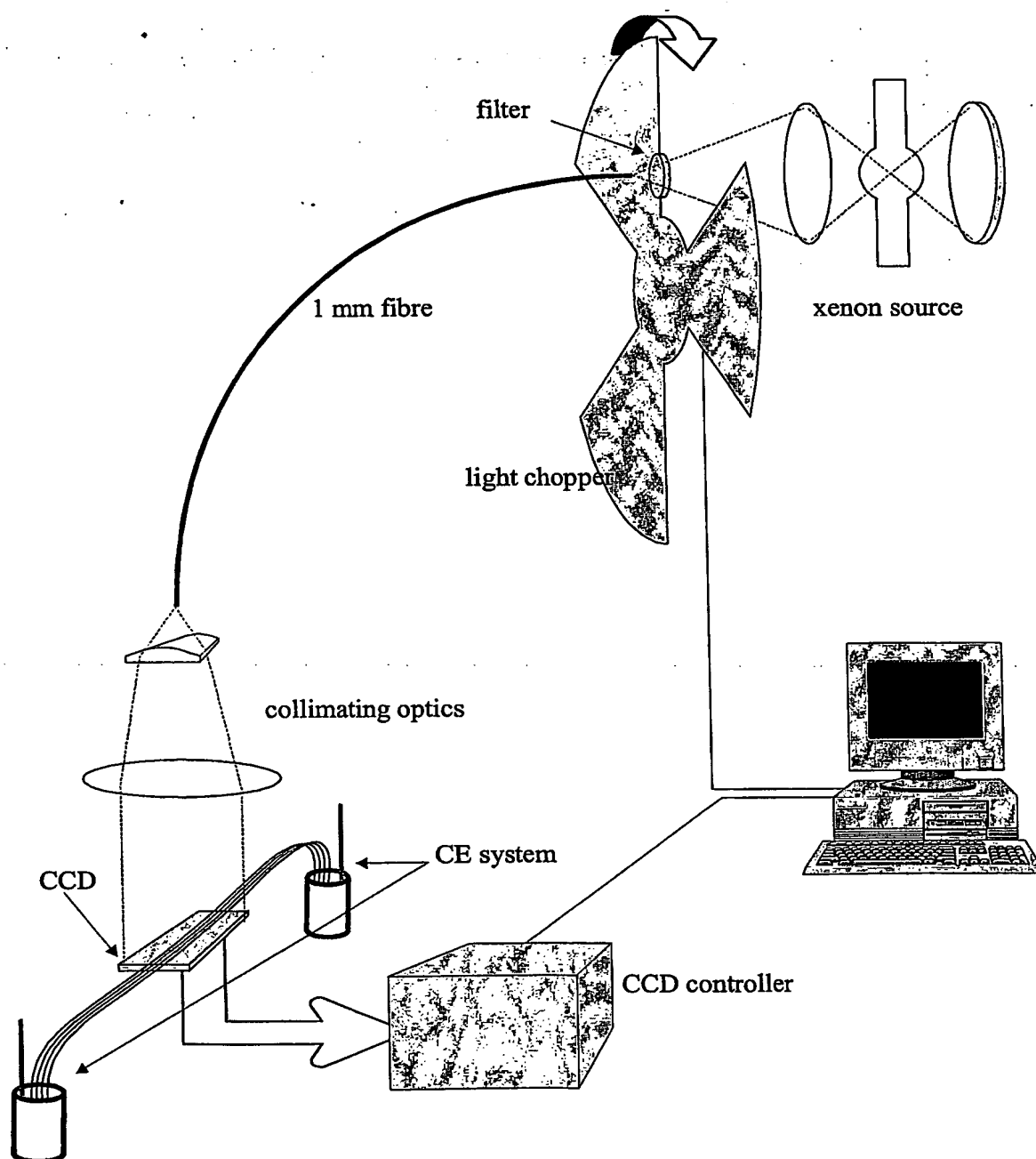
10 44. Assembly, method, module, clip-on device or use thereof substantially as herein described or illustrated in the description, the examples and/or the figures.

1 / 17

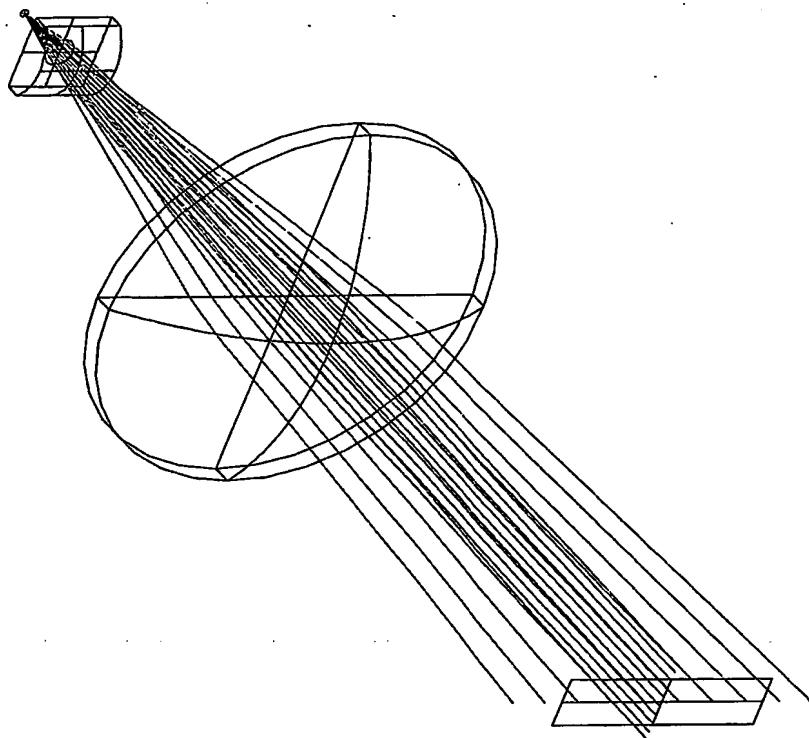


*Fig. A*

2/17

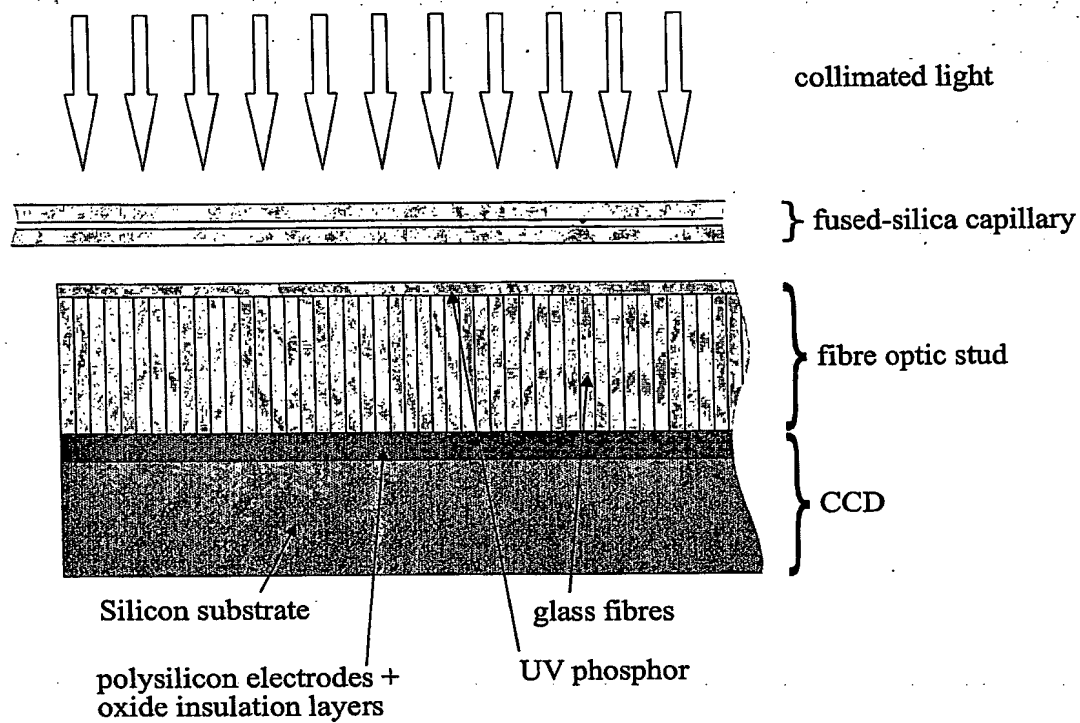


**Figure 1.** Schematic diagram of experimental apparatus for parallel capillary absorbance detection.



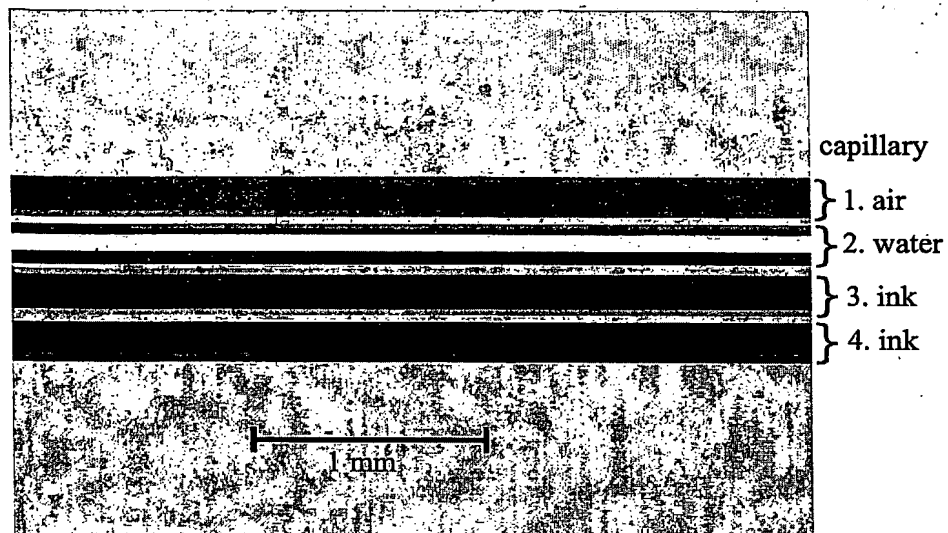
**Figure 2.** Collimated illumination of rectangular CCD area, (26.6 x 6.7 mm) using light output from a 1 mm diameter fused-silica optical fibre (N.A. = 0.22) using a cylindrical and spherical fused-silica lens elements.

4/17



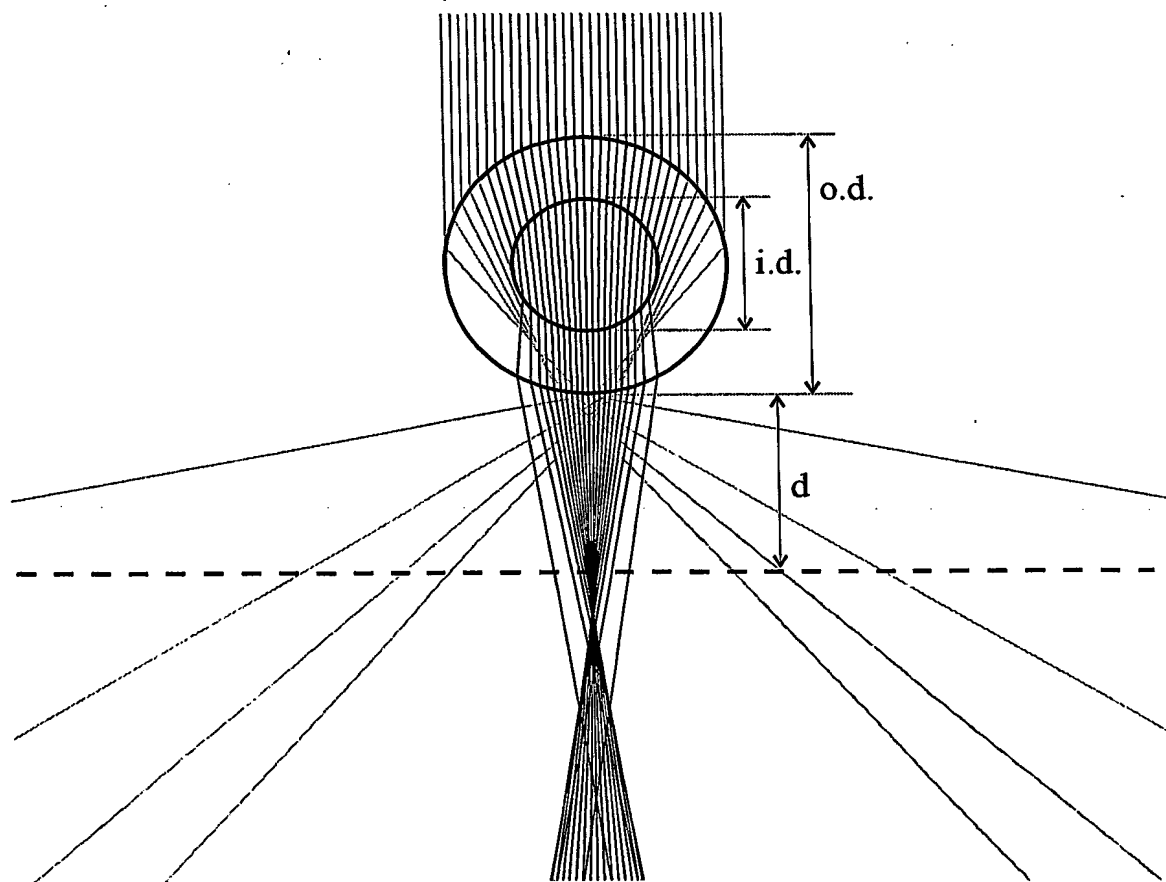
**Figure 3.** Detail of CCD with fibre optic stud and imaging of capillaries.

5/17



**Figure 4.** Part of one CCD snapshot showing ~3 mm of 4 capillaries (100  $\mu\text{m}$  i.d., 194  $\mu\text{m}$  o.d.); the total area imaged is  $6.7 \times 26.6$  mm. The contents of the capillaries are, 1. air, 2. water, 3 & 4 ink solution.

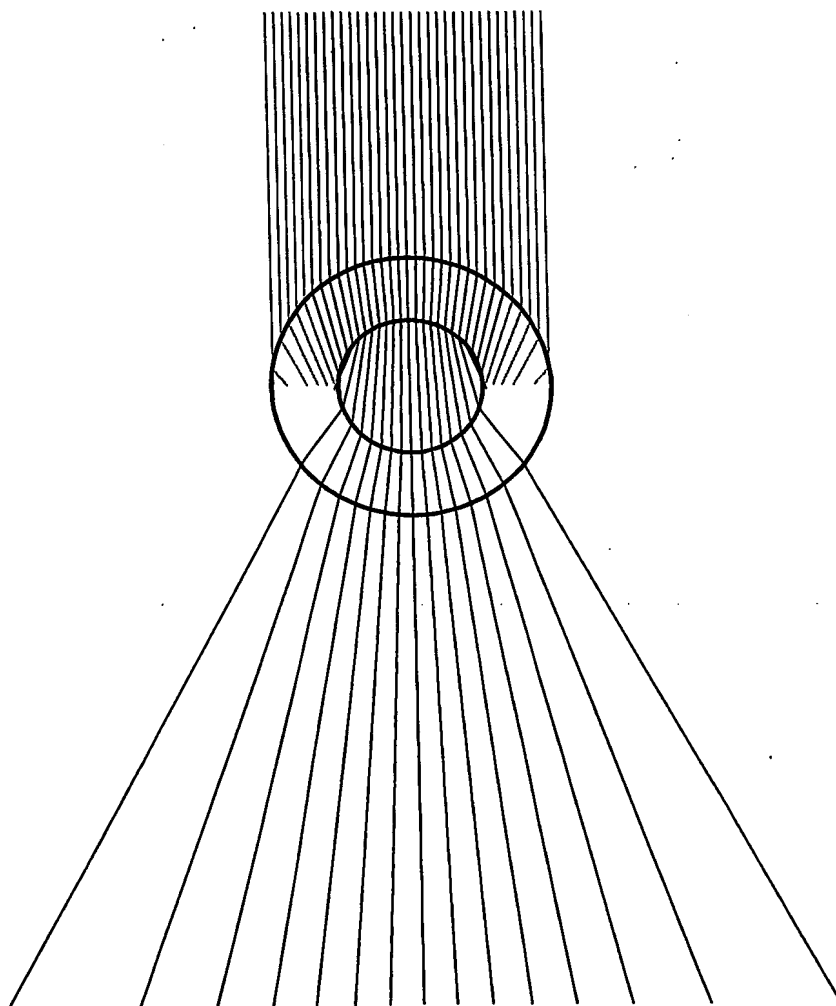
6/17



**Figure 5.** Water-filled capillary 100  $\mu\text{m}$  i.d., 194  $\mu\text{m}$  o.d. .

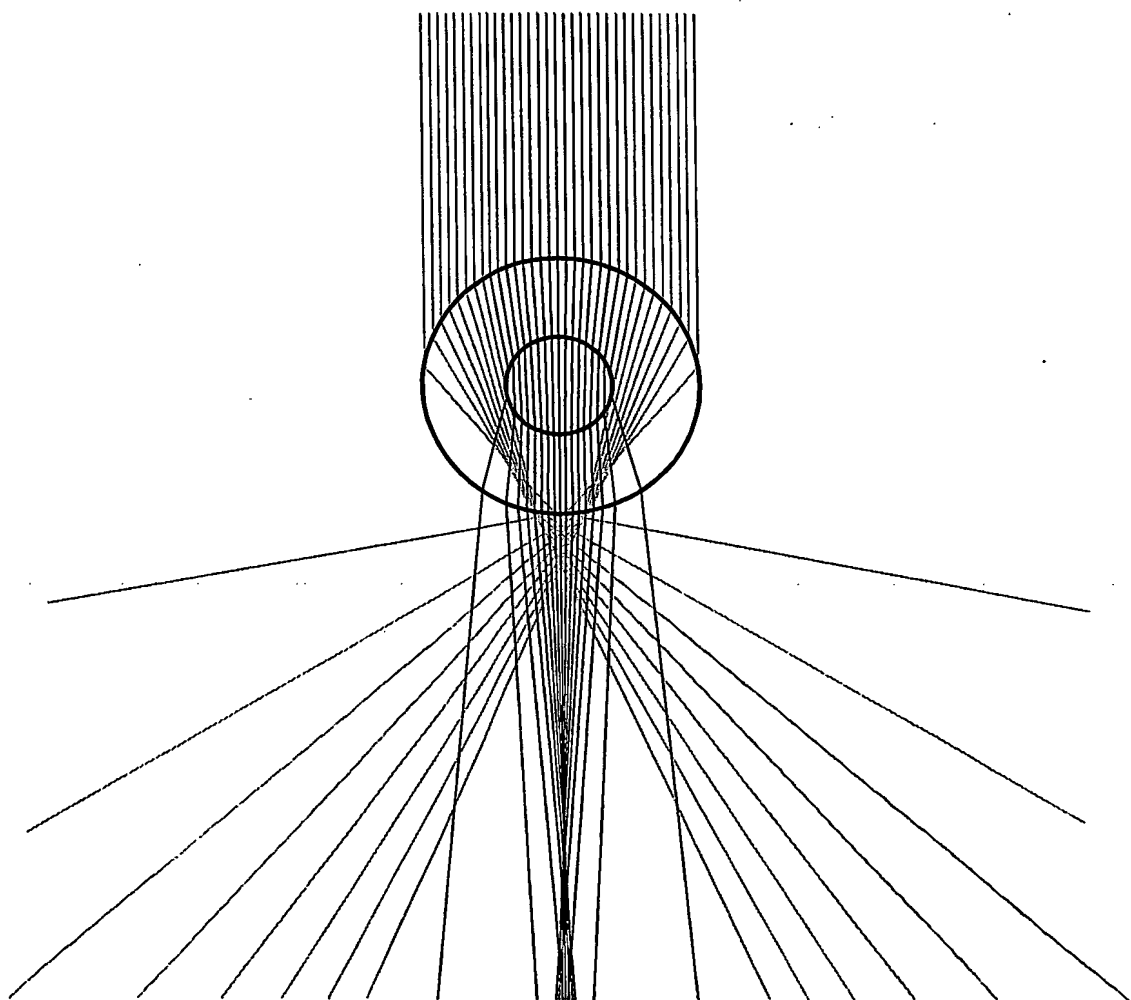


7/17



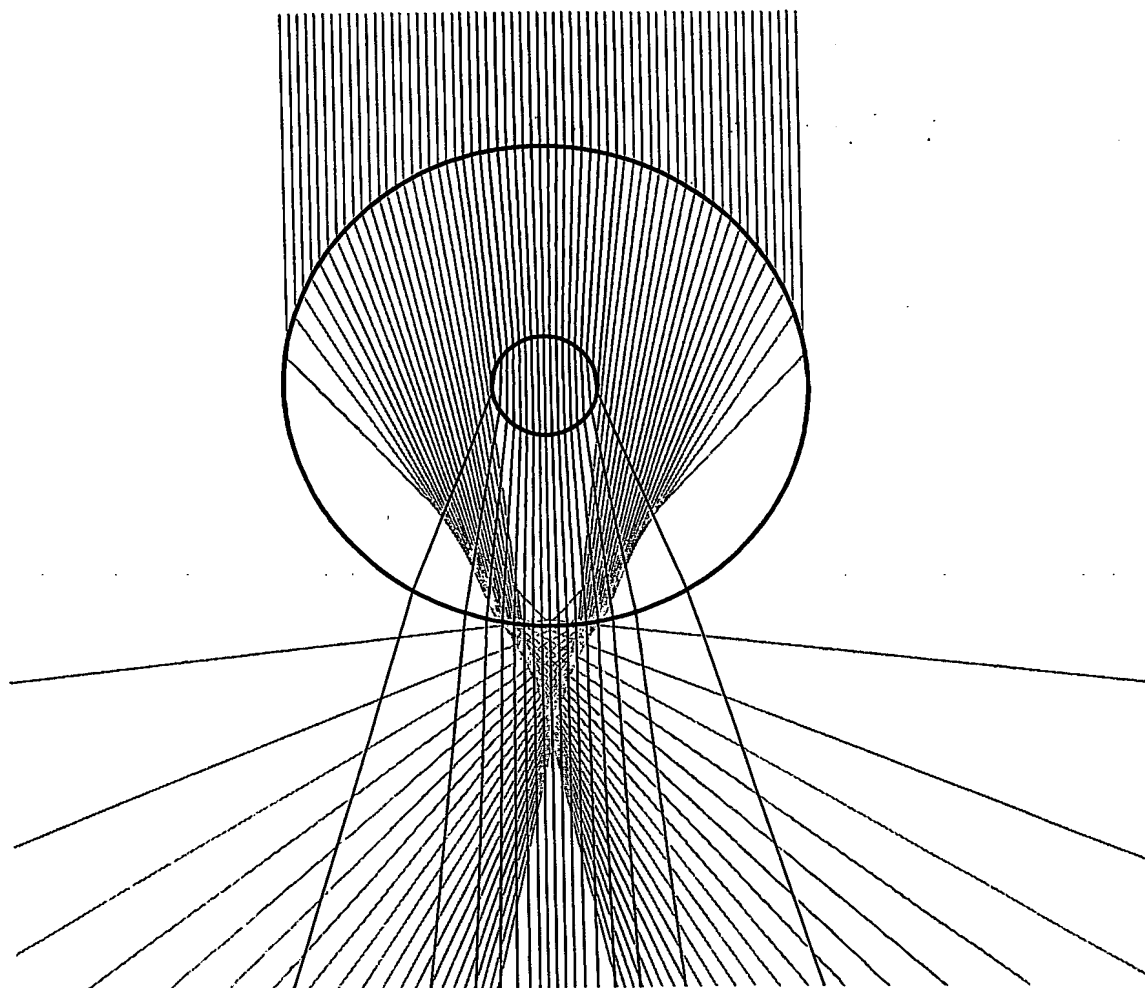
**Figure 6.** Air filled capillary, 100 μm i.d., 194 μm o.d.

8/17



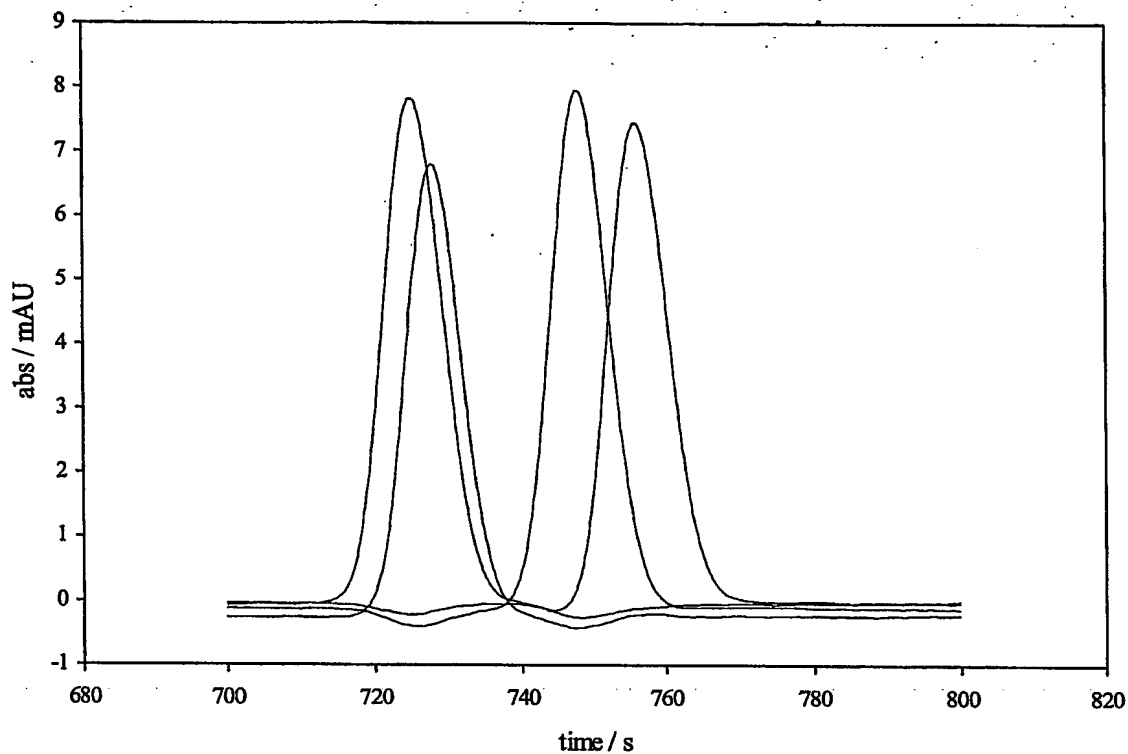
**Figure 7.** Water filled capillary, 75  $\mu\text{m}$  i.d., 194  $\mu\text{m}$  o.d.

9/17



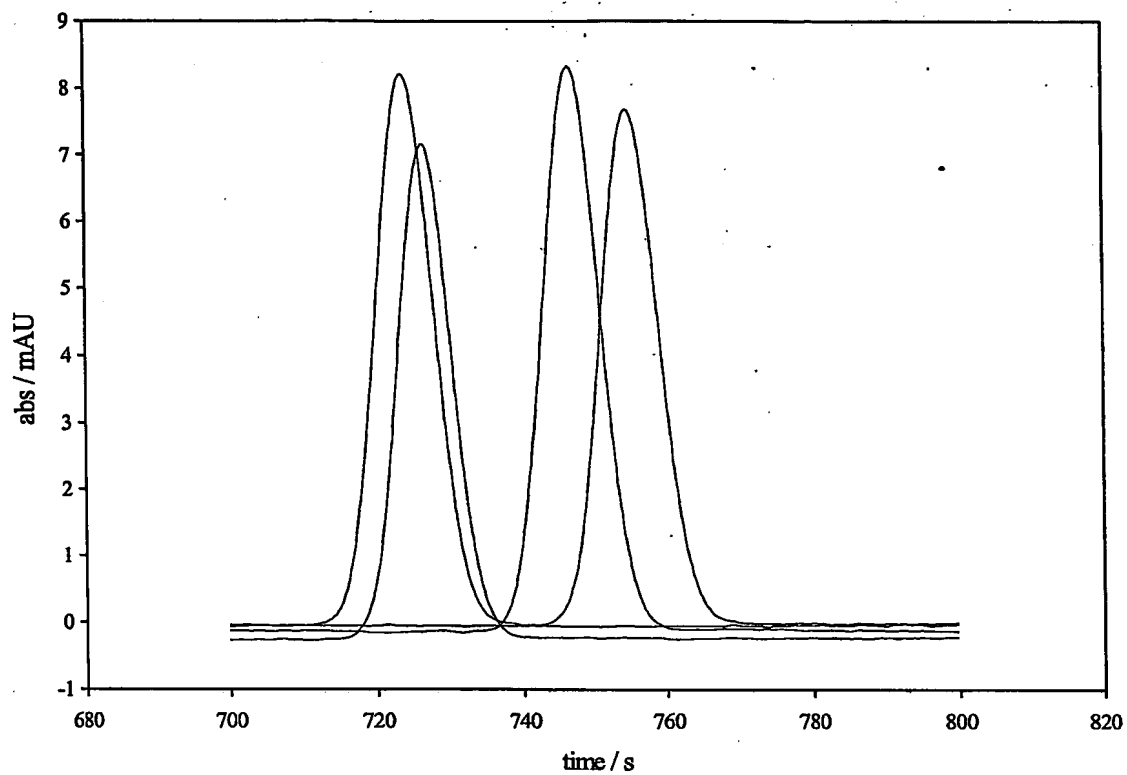
**Figure 8.** Water filled capillary, 75  $\mu\text{m}$  i.d., 364  $\mu\text{m}$  o.d.

10/17



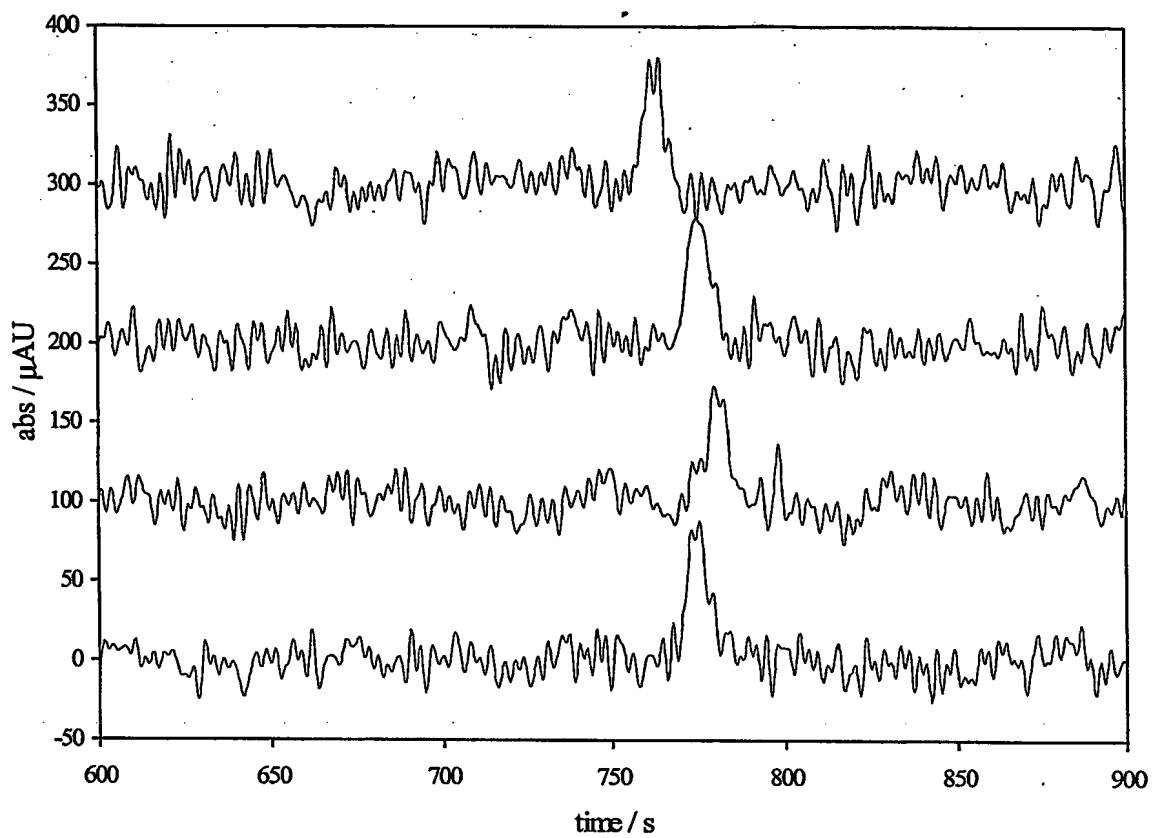
**Figure 9.** Electropherograms of ~16 nL 100  $\mu$ M p-nitrophenol injected into each of four parallel 100  $\mu$ m i.d. capillaries. Capillary length: 500 mm total, 300 mm to the detector. Separation voltage: 5000 V. Buffer: sodium phosphate pH 7.5 (15 mM sodium).

11/17



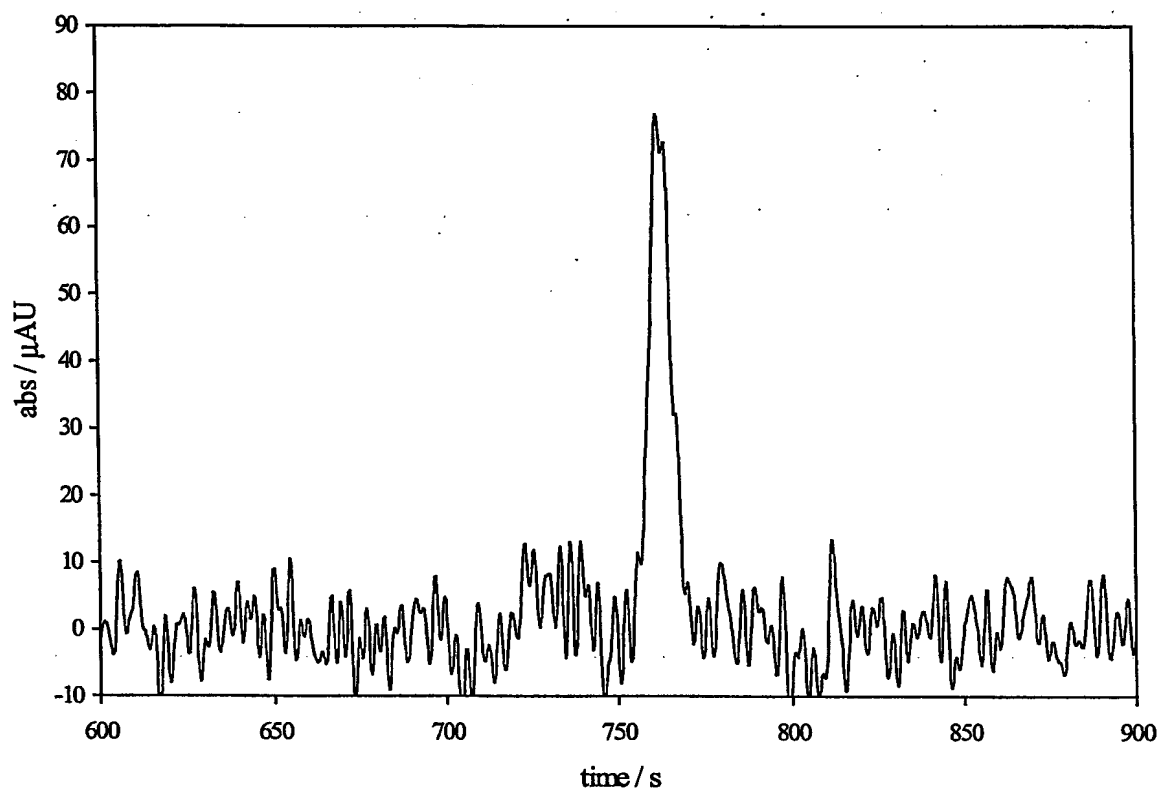
**Figure 10.** Electropherograms of 100  $\mu$ M p-nitrophenol after correction for cross-talk between capillaries.

12/17



**Figure 11.** Electropherograms of ~16 nL 1  $\mu$ M p-nitrophenol injected into each capillary.

13/17



**Figure 12.** Electropherogram generated by taking the average of the four traces shown in figure 11.

14/17

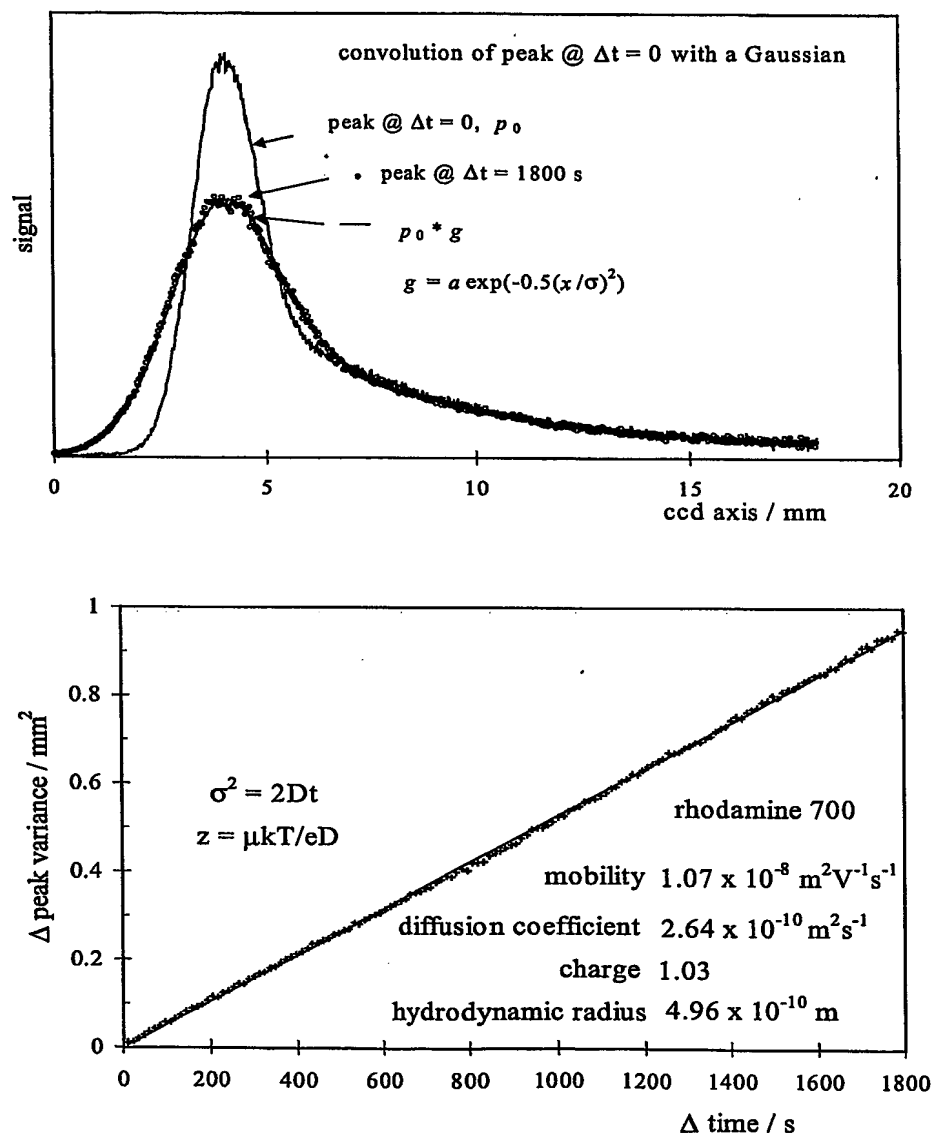
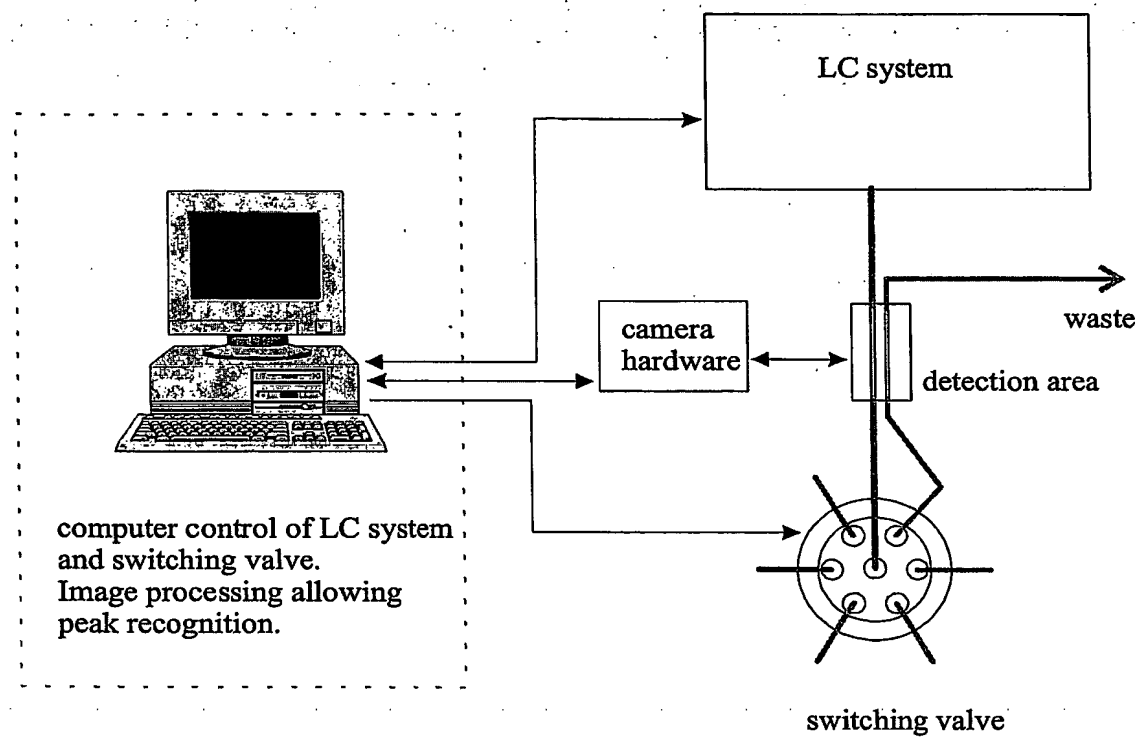


Figure 13



15/17

**Figure 14.**

16/17

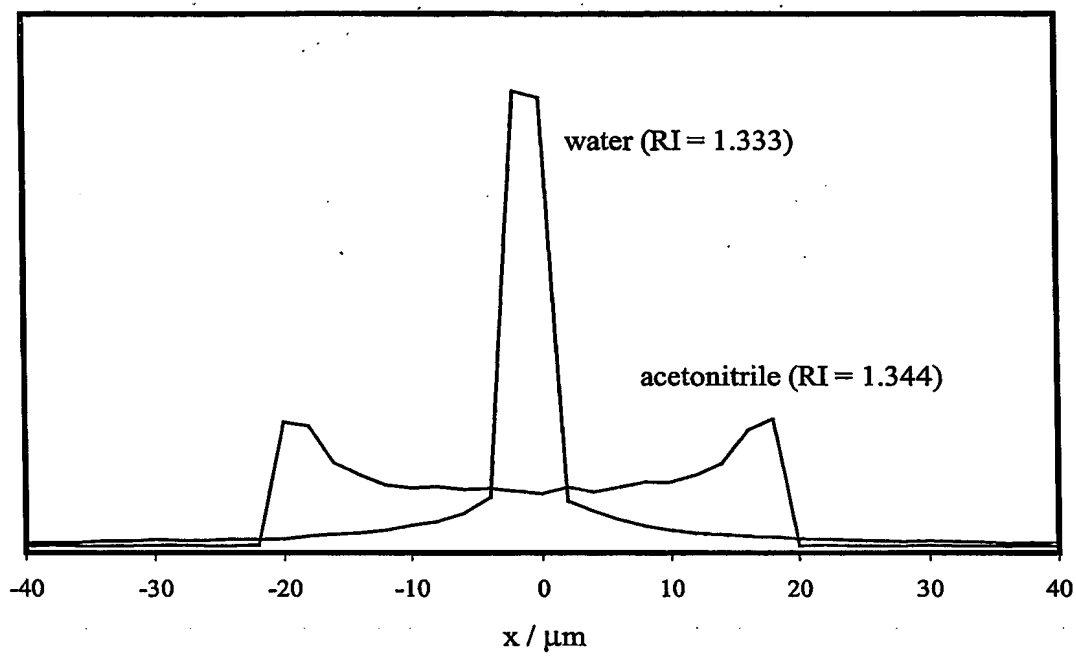
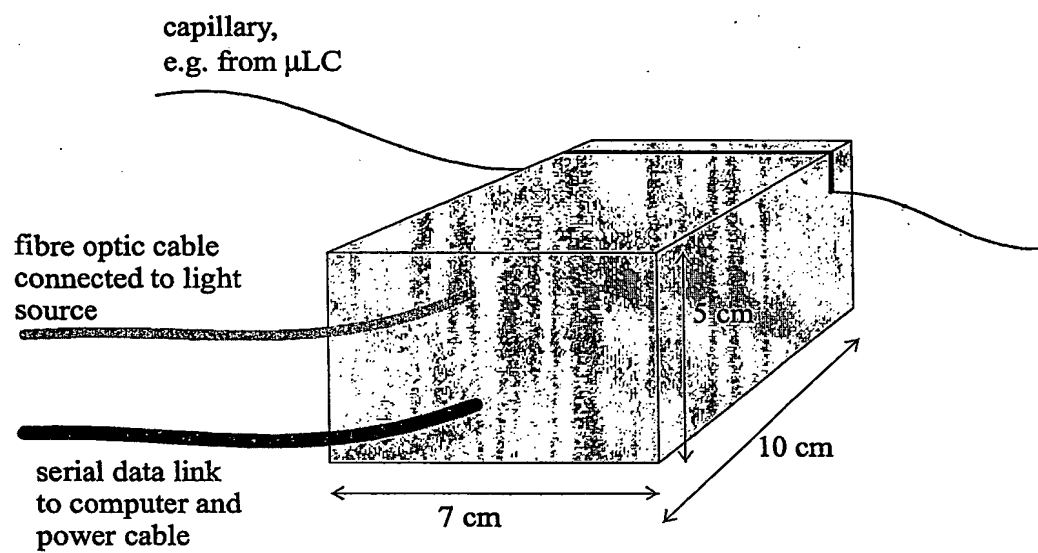


Figure 15.

17/17

**Figure 16.**

## INTERNATIONAL SEARCH REPORT

Internationa Application No

PCT/GB 03/03591

A. CLASSIFICATION OF SUBJECT MATTER  
IPC 7 G01N27/447 G01N21

According to International Patent Classification (IPC) or to both national classification and IPC

## B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC 7 G01N

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EPO-Internal, WPI Data, PAJ

## C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	EP 0 616 211 A (CIBA GEIGY AG) 21 September 1994 (1994-09-21)	1,24
Y	column 5, line 13 -column 7, line 53; figure 3	1,24
A		3,5-9, 11-16, 25-31,35
Y	US 5 694 215 A (CARVER DAVID R) 2 December 1997 (1997-12-02)	1,24
A	column 6, line 20 -column 8, line 14; figures 2,4,5	2,5-9, 11-13, 15,16, 20,22, 25-30
	--- -/--	

☒ Further documents are listed in the continuation of box C.☒ Patent family members are listed in annex.

## \* Special categories of cited documents:

- \*A\* document defining the general state of the art which is not considered to be of particular relevance
- \*E\* earlier document but published on or after the international filing date
- \*L\* document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
- \*O\* document referring to an oral disclosure, use, exhibition or other means
- \*P\* document published prior to the international filing date but later than the priority date claimed

- \*T\* later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
- \*X\* document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
- \*Y\* document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.
- \*Z\* document member of the same patent family

Date of the actual completion of the international search

17 December 2003

Date of mailing of the international search report

13/01/2004

Name and mailing address of the ISA

European Patent Office, P.B. 5818 Patentlaan 2  
NL - 2280 HV Rijswijk  
Tel. (+31-70) 340-2040, Tx. 31 651 epo nl,  
Fax: (+31-70) 340-3016

Authorized officer

Stuebner, B

## INTERNATIONAL SEARCH REPORT

Internationale

Application No

PCT/GB 03/03591

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT		
Category °	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	BRUNO A E ET AL: "ON-COLUMN CAPILLARY FLOW CELL UTILIZING OPTICAL WAVEGUIDES FOR CHROMATOGRAPHIC APPLICATIONS" ANALYTICAL CHEMISTRY, AMERICAN CHEMICAL SOCIETY, COLUMBUS, US, vol. 61, no. 8, 15 April 1989 (1989-04-15), pages 876-883, XP000081371 ISSN: 0003-2700 page 877, column 1, paragraph 3 -page 879, column 1, paragraph 3; figure 2 ---	1,3,12, 13,15,16
A	E.T. BERGSTRÖM ET AL: "A Charged Coupled Device Array Detector for Single-Wavelength and Multiwavelength Ultraviolet Absorbance in Capillary Electrophoresis" ANALYTICAL CHEMISTRY, vol. 71, no. 19, October 1999 (1999-10), pages 4376-4384, XP002265488 page 4378 -page 4379; figure 2 ---	1,7,24
A	US 5 239 360 A (MORING STEPHEN E ET AL) 24 August 1993 (1993-08-24) figure 1 ---	1,24
A	EP 0 594 327 A (APPLIED BIOSYSTEMS) 27 April 1994 (1994-04-27) page 5, line 37 -page 7, line 9; figure 2 -----	1,24

# INTERNATIONAL SEARCH REPORT

Int'l Application No.  
PCT/ISA/210 03/03591

## Box I Observations where certain claims were found unsearchable (Continuation of item 1 of first sheet)

This International Search Report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. ☐ Claims Nos.:  
because they relate to subject matter not required to be searched by this Authority, namely:
2. ☒ Claims Nos.: 39  
because they relate to parts of the International Application that do not comply with the prescribed requirements to such an extent that no meaningful International Search can be carried out, specifically:  
see FURTHER INFORMATION sheet PCT/ISA/210
3. ☐ Claims Nos.:  
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

## Box II Observations where unity of invention is lacking (Continuation of item 2 of first sheet)

This International Searching Authority found multiple inventions in this International application, as follows:

1. ☐ As all required additional search fees were timely paid by the applicant, this International Search Report covers all searchable claims.
2. ☐ As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment of any additional fee.
3. ☐ As only some of the required additional search fees were timely paid by the applicant, this International Search Report covers only those claims for which fees were paid, specifically claims Nos.:
4. ☐ No required additional search fees were timely paid by the applicant. Consequently, this International Search Report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

### Remark on Protest

- ☐ The additional search fees were accompanied by the applicant's protest.
- ☐ No protest accompanied the payment of additional search fees.

FURTHER INFORMATION CONTINUED FROM PCT/ISA/ 210

Continuation of Box I.2

Claims Nos.: 39

Claim 39 relies on references to the description and figures in contradiction to Rule 6.2a) PCT.

The applicant's attention is drawn to the fact that claims, or parts of claims, relating to inventions in respect of which no international search report has been established need not be the subject of an international preliminary examination (Rule 66.1(e) PCT). The applicant is advised that the EPO policy when acting as an International Preliminary Examining Authority is normally not to carry out a preliminary examination on matter which has not been searched. This is the case irrespective of whether or not the claims are amended following receipt of the search report or during any Chapter II procedure.

# INTERNATIONAL SEARCH REPORT

Intern: Application No

PCT/GB 03/03591

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
EP 0616211	A	21-09-1994	EP 0616211 A1 21-09-1994
		DE 69323060 D1	25-02-1999
		DE 69323060 T2	10-06-1999
		JP 6300690 A	28-10-1994
		US 5636017 A	03-06-1997
US 5694215	A	02-12-1997	NONE
US 5239360	A	24-08-1993	NONE
EP 0594327	A	27-04-1994	US 5274227 A 28-12-1993
		DE 69331619 D1	04-04-2002
		DE 69331619 T2	17-10-2002
		EP 0594327 A1	27-04-1994
		JP 3186375 B2	11-07-2001
		JP 7049340 A	21-02-1995



**This Page is Inserted by IFW Indexing and Scanning  
Operations and is not part of the Official Record**

**BEST AVAILABLE IMAGES**

Defective images within this document are accurate representations of the original documents submitted by the applicant.

Defects in the images include but are not limited to the items checked:

- ☐ BLACK BORDERS
- ☐ IMAGE CUT OFF AT TOP, BOTTOM OR SIDES
- ☐ FADED TEXT OR DRAWING
- ☒ BLURRED OR ILLEGIBLE TEXT OR DRAWING
- ☐ SKEWED/SLANTED IMAGES
- ☐ COLOR OR BLACK AND WHITE PHOTOGRAPHS
- ☐ GRAY SCALE DOCUMENTS
- ☒ LINES OR MARKS ON ORIGINAL DOCUMENT
- ☐ REFERENCE(S) OR EXHIBIT(S) SUBMITTED ARE POOR QUALITY
- ☐ OTHER: \_\_\_\_\_

**IMAGES ARE BEST AVAILABLE COPY.**

**As rescanning these documents will not correct the image problems checked, please do not report these problems to the IFW Image Problem Mailbox.**